

Neural Tractography Using an Unscented Kalman Filter

Proceedings page 126

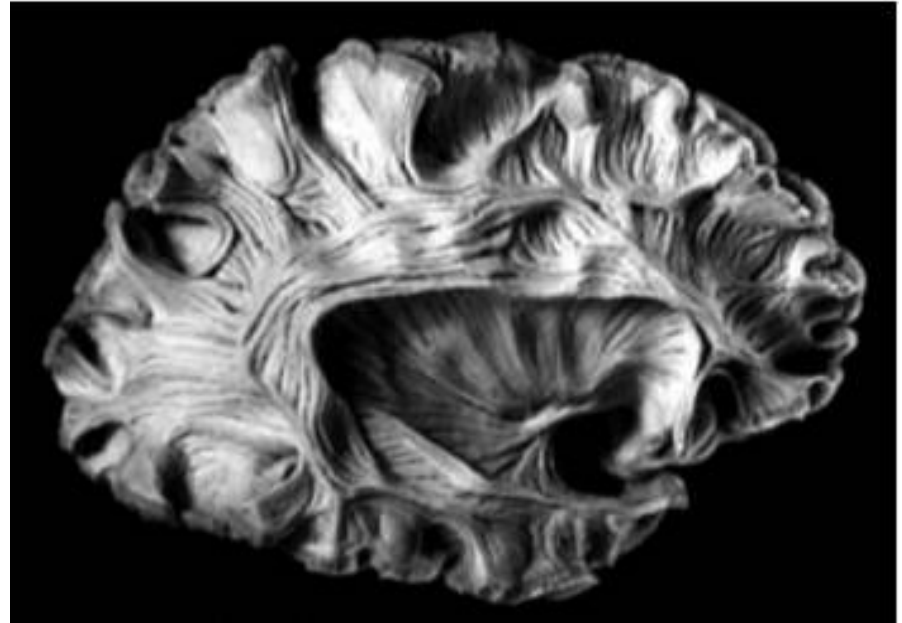
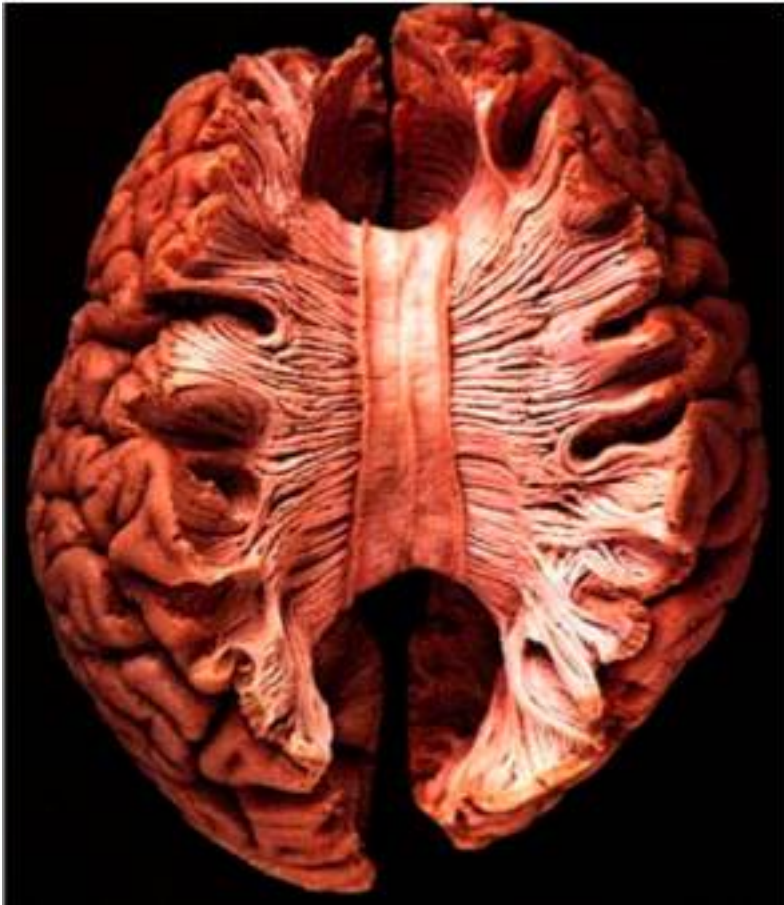
James Malcolm

Advisor: Yogesh Rathi
Psychiatry Neuroimaging Lab.
Harvard Medical School

Presented at “Information Processing in Medical Imaging”, 7 July 2009

background

neural fibers

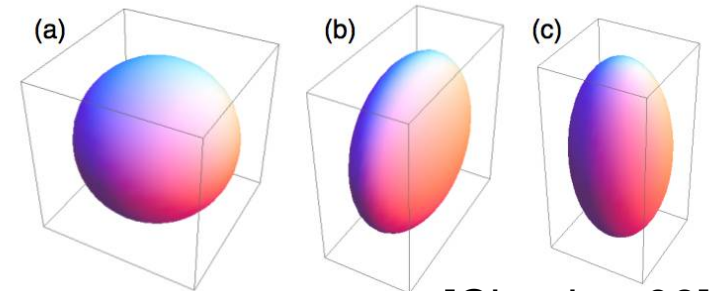


[Williams 97]

imaging techniques

- Diffusion tensor imaging (DTI)

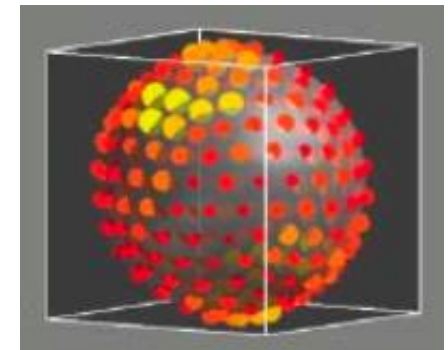
- [Basser 94]



[Clayden 08]

- High Angular Resolution (QBI)

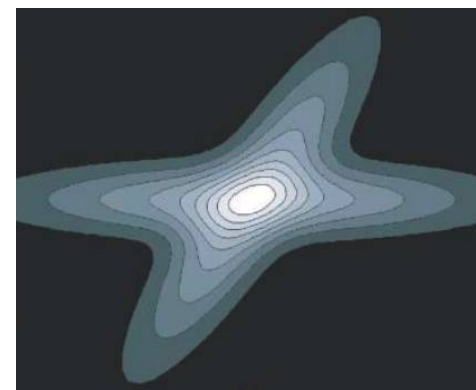
- [Tuch 02]



[Tuch 04]

- Diffusion Spectrum (DSI)

- [Wedeen 05, Hagmann 05]

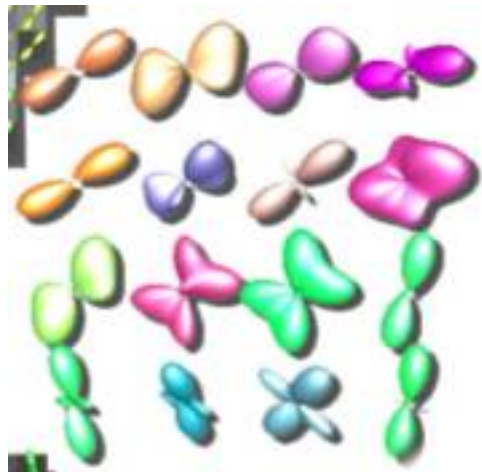
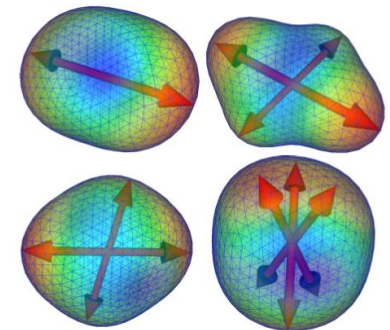
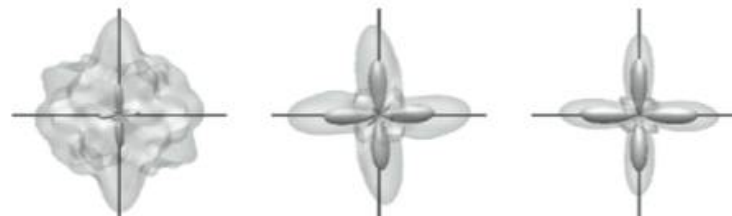
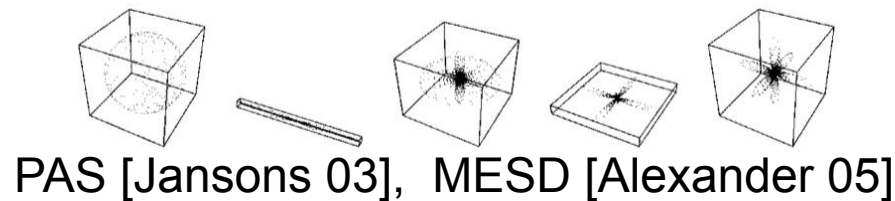


[Hagmann 05]

voxel reconstruction



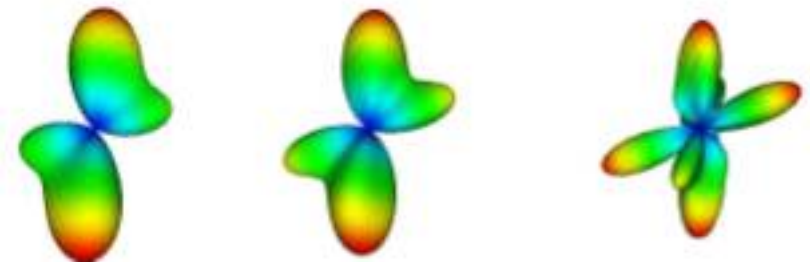
tensor mixtures [Tuch 02]



VMF [Kumar 08]



DOT [Ozarslan 05]



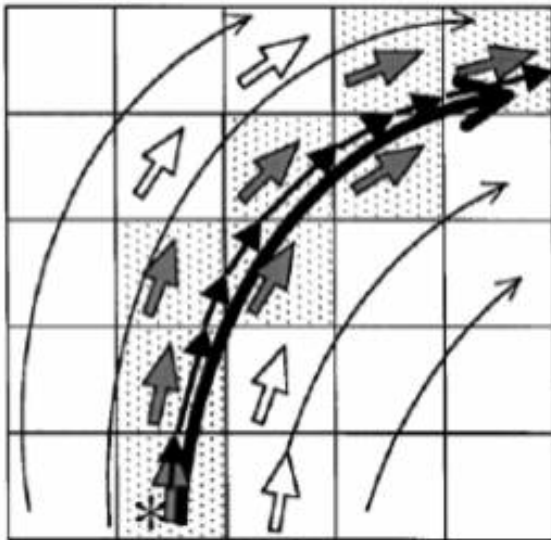
spherical harmonics [Descoteaux 07]



Wishart [Jian 07]

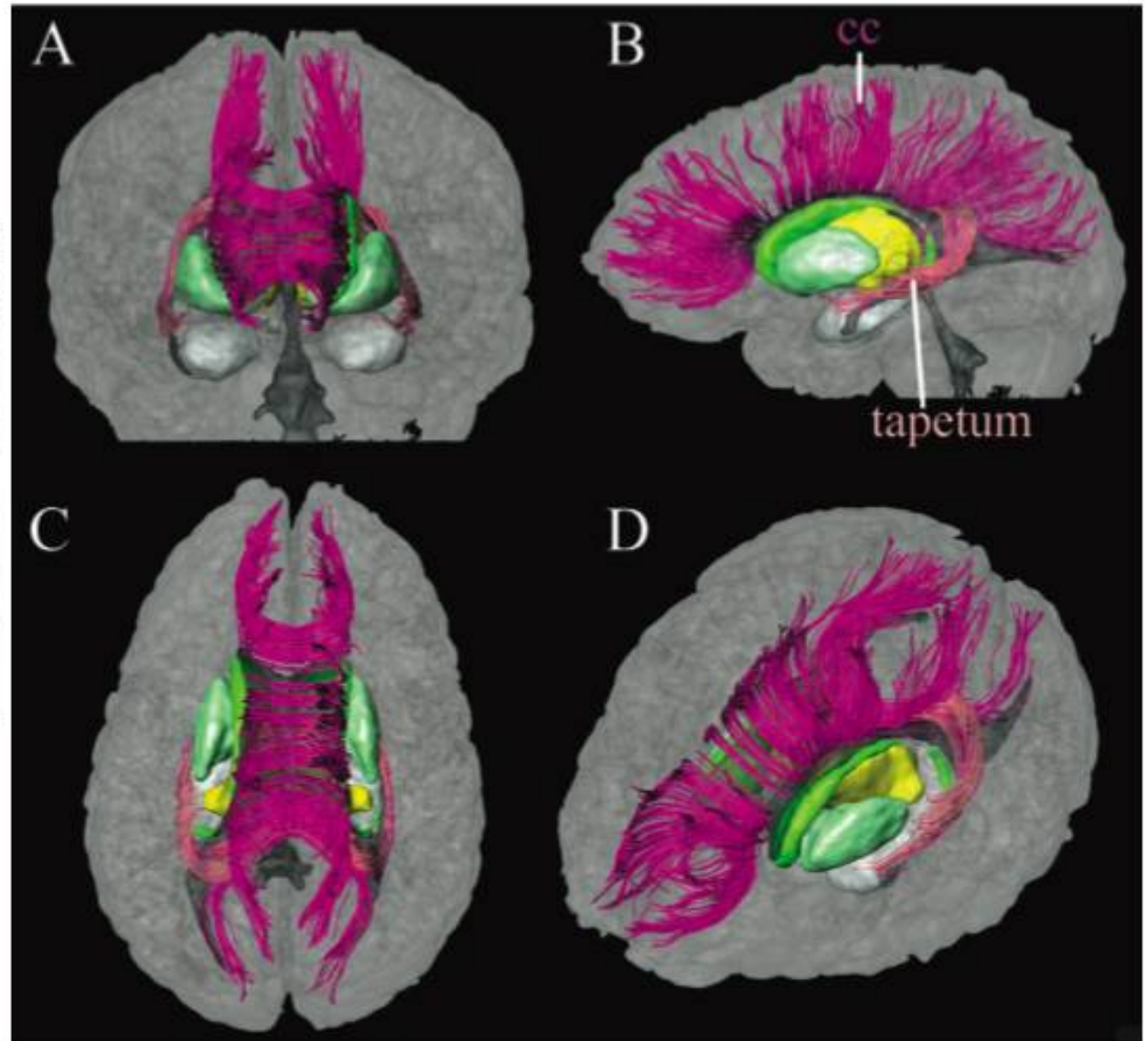
deterministic tractography

streamline



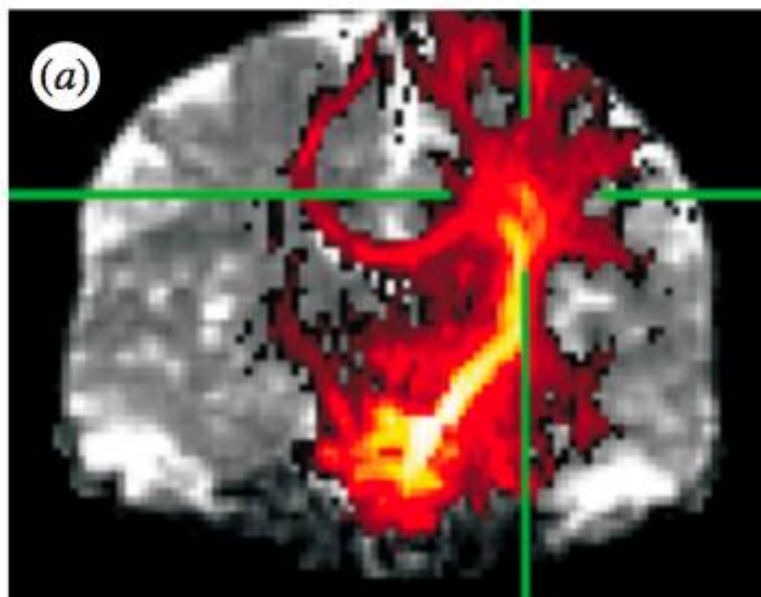
[Mori 99]

[Conturo 99, Basser 00]

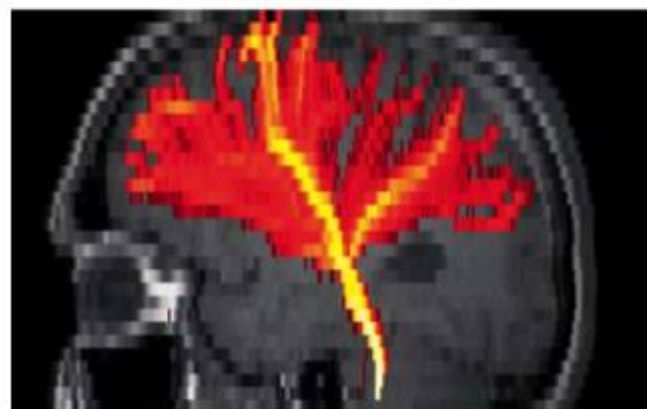
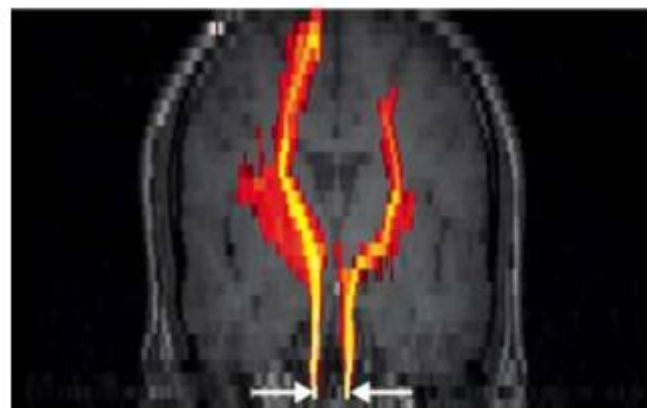


[Wakana 03]

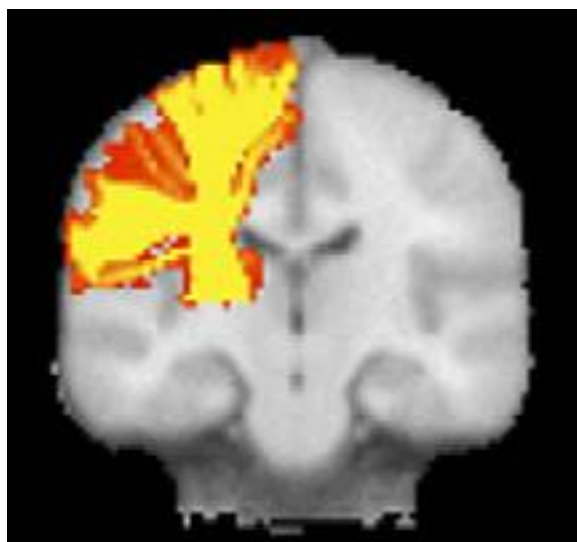
probabilistic tractography



[Parker 05]

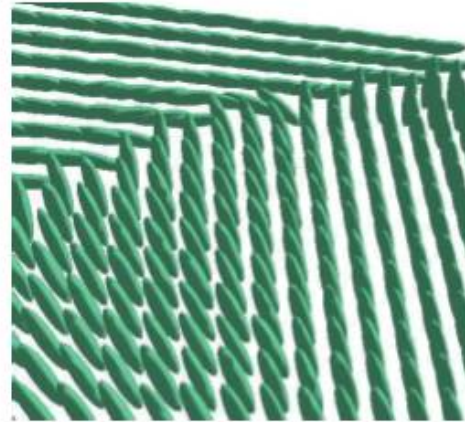
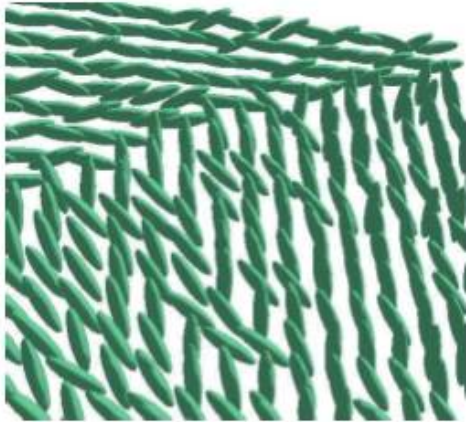


[Friman 06]



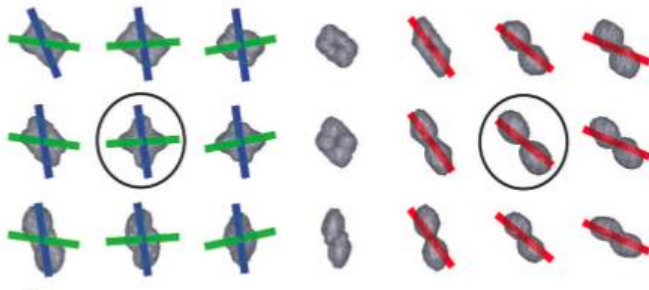
[Behrens 07]

spatial regularization

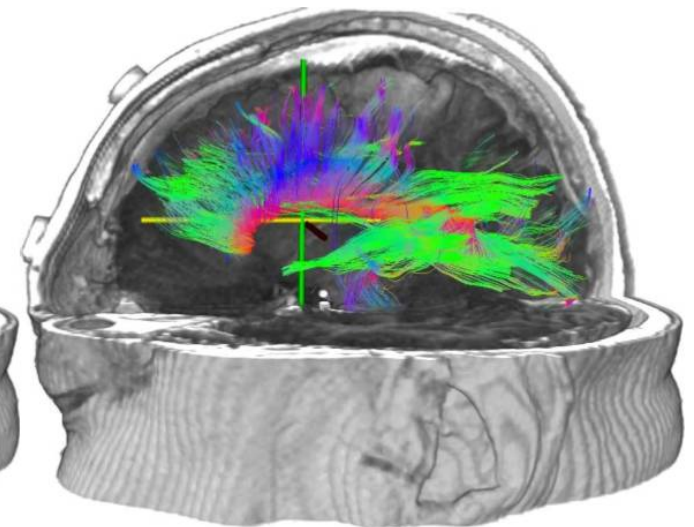
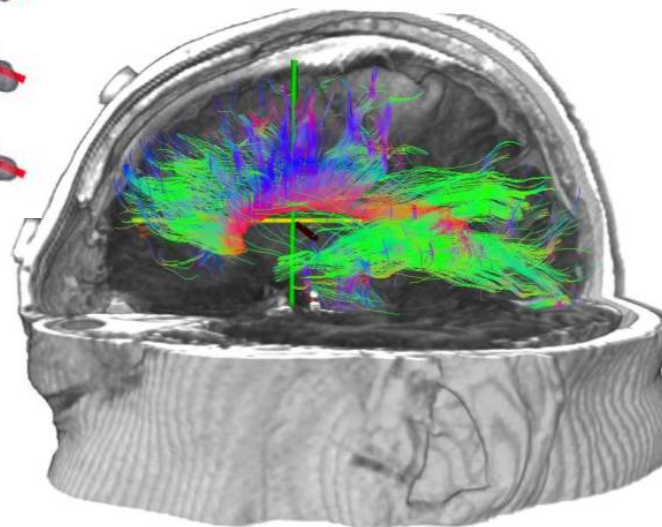


pre/post-processing

[Tschumperle 03]



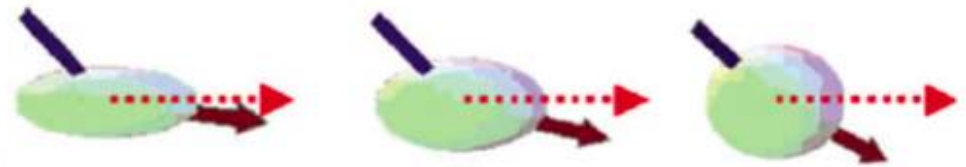
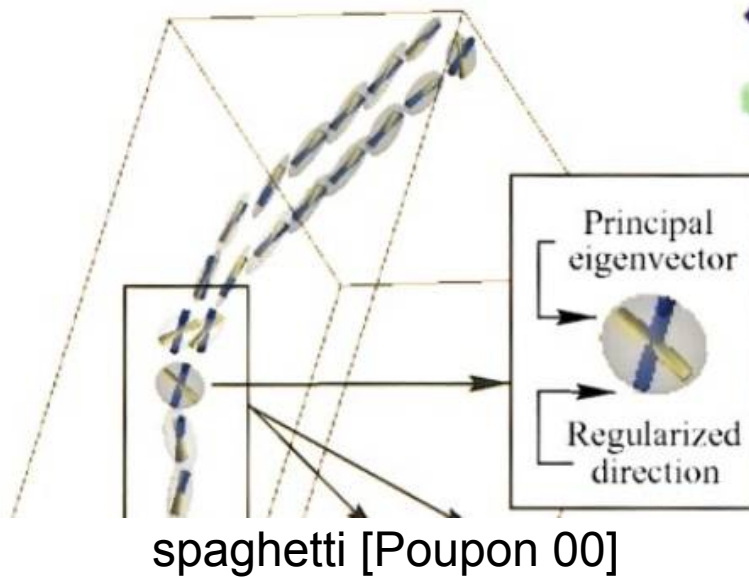
[Savadjiev 07]



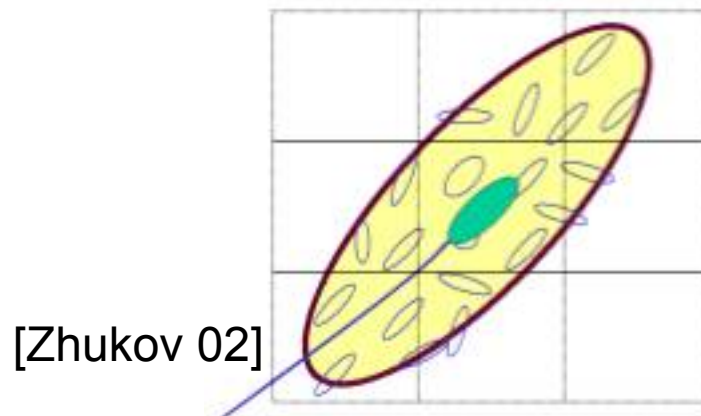
[Fillard 07]

tract regularization

deterministic approaches:



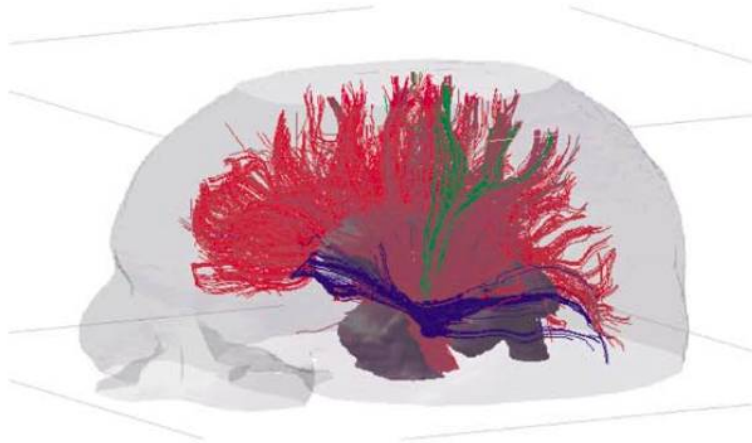
deflection [Lazar 03]



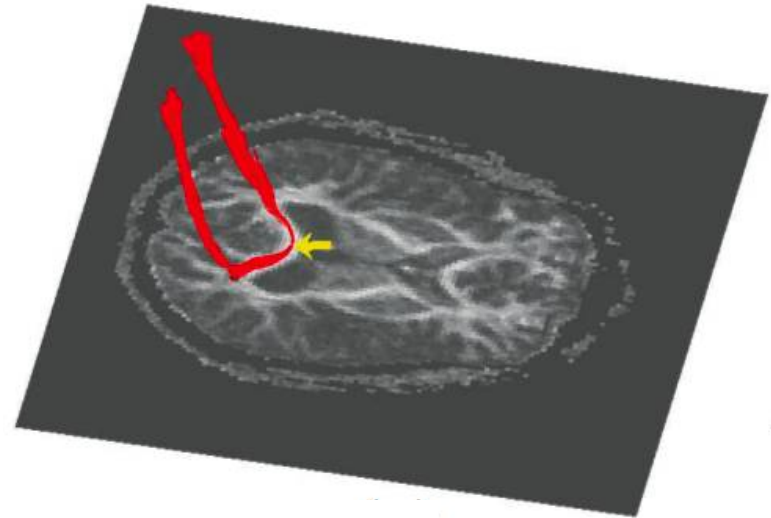
single-tensor
path regularization

tract regularization

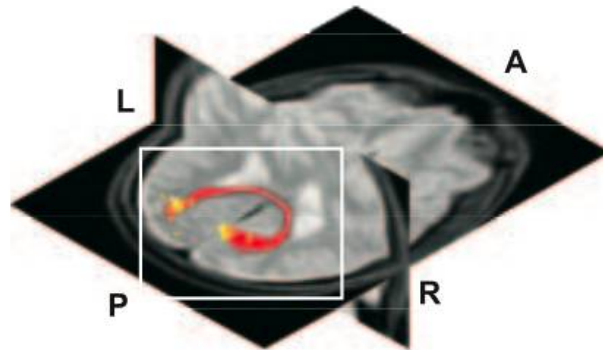
probabilistic approaches:



linear Kalman filter [Gossl 02]



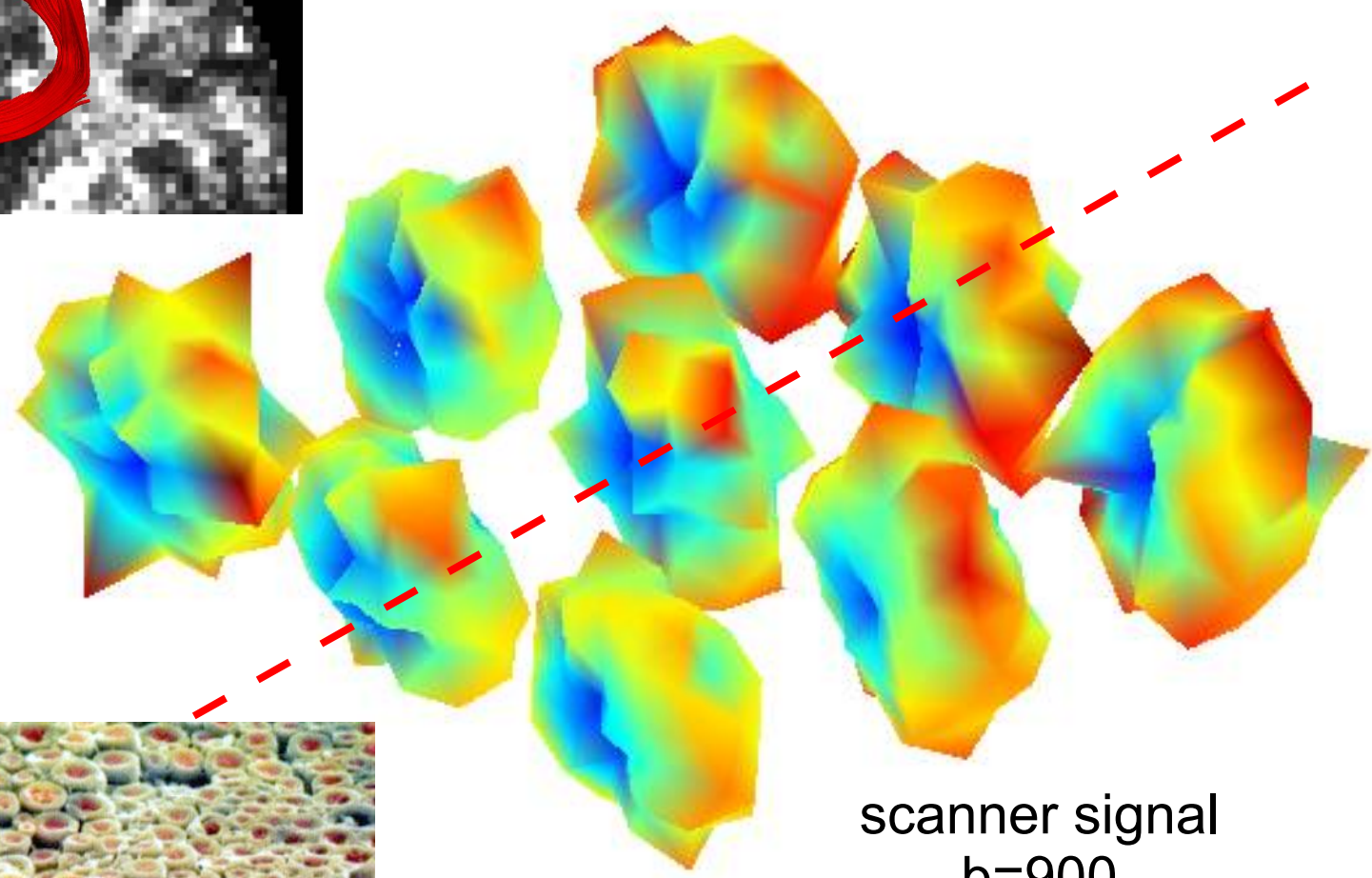
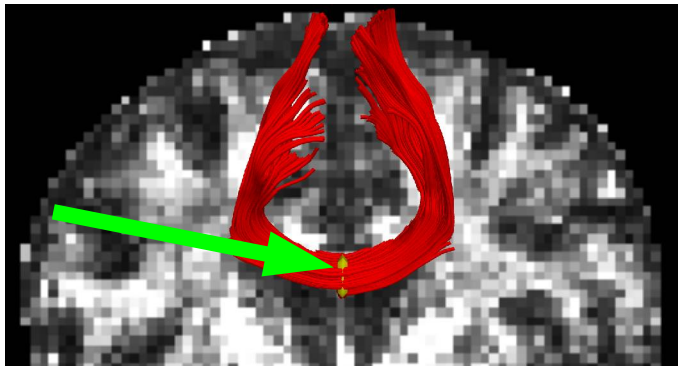
particle filtering [Zhang 07]



stochastic [Bjornemo 02]

single-tensor
path regularization

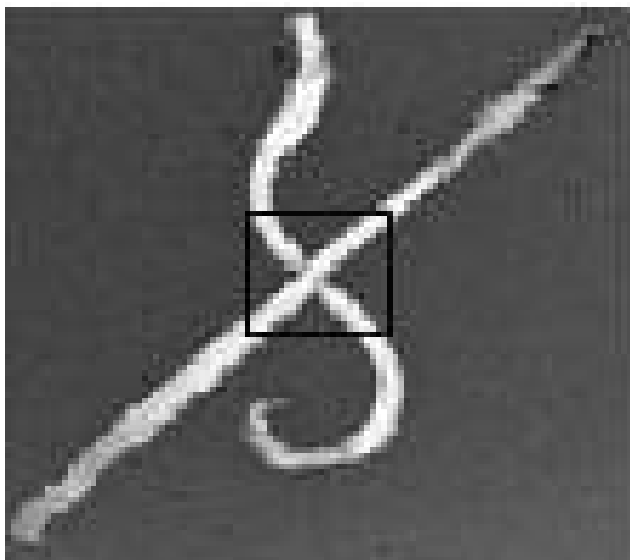
method:
the model



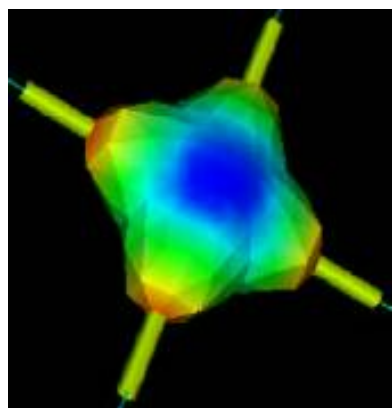
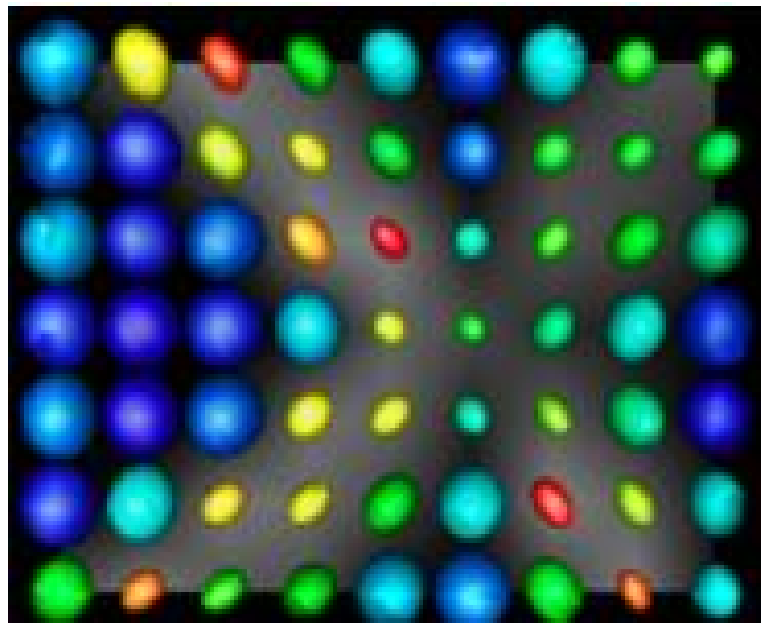
scanner signal
b=900
51 directions
1.7mm isotropic voxel
17 minute scan

[Bartzokis]

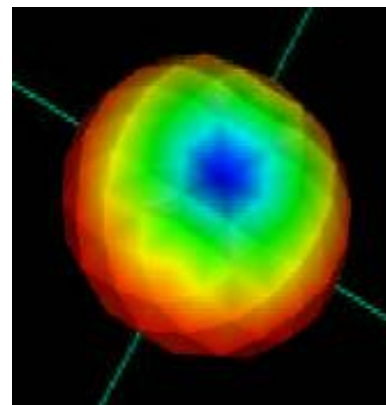
single-tensor limitations



rat spinal nerves



true ODF



single-tensor ODF

[Campbell 05, Descoteaux 06]

[Descoteaux 06]

multi-tensor signal model

$$S(\mathbf{u}) = s_0 \sum_j w_j e^{-b \mathbf{u}^T D_j \mathbf{u}}$$

D_j diffusion tensor

$\mathbf{u}$ unit direction

w_j convex weights

b acquisition constant

s_0 null signal ($b=0$)

model assumptions

...in this study

Two fibers

Fixed volume fractions

Tensors are elliptic or isotropic

model parameters

for two fibers...

...two principal directions $\mathbf{m} \in \mathbb{R}^3$

...two primary eigenvalues $\lambda_1 \in \mathbb{R}$

...two minor eigenvalues $\lambda_2 \in \mathbb{R}$

5 + 5 = 10 parameters

model parameters

for two fibers...

...two principal directions $\mathbf{m} \in \mathbb{R}^3$

...two primary eigenvalues $\lambda_1 \in \mathbb{R}$

...two minor eigenvalues $\lambda_2 \in \mathbb{R}$

5 + 5 = 10 parameters

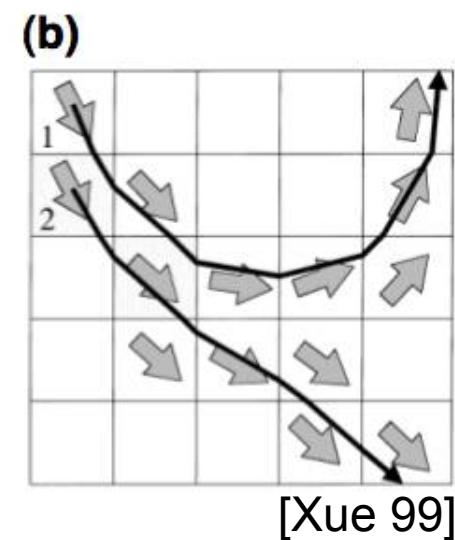
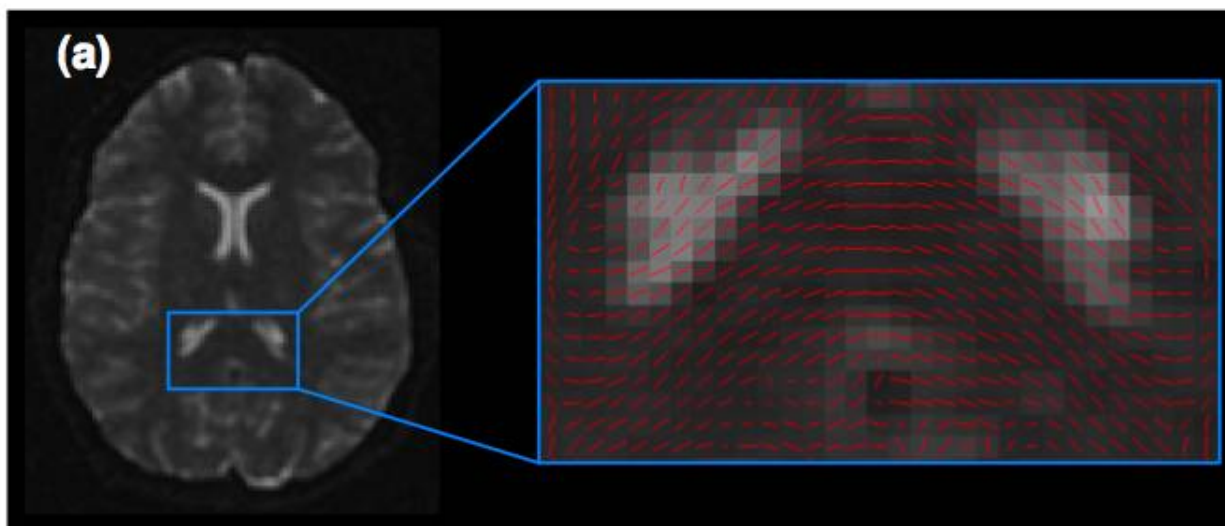
$$S(\mathbf{u}) = 0.5 s_0 e^{-b \mathbf{u}^T D_1 \mathbf{u}} + 0.5 s_0 e^{-b \mathbf{u}^T D_2 \mathbf{u}}$$

$$D_1 = \lambda_{11} \mathbf{m}_1 \mathbf{m}_1^T + \lambda_{21} (\mathbf{p} \mathbf{p}^T + \mathbf{q} \mathbf{q}^T)$$

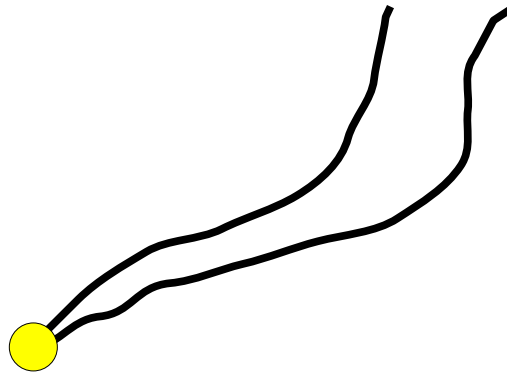
eigenvectors: $\mathbf{m}$, $\mathbf{p}$, $\mathbf{q}$

method:
estimating the model

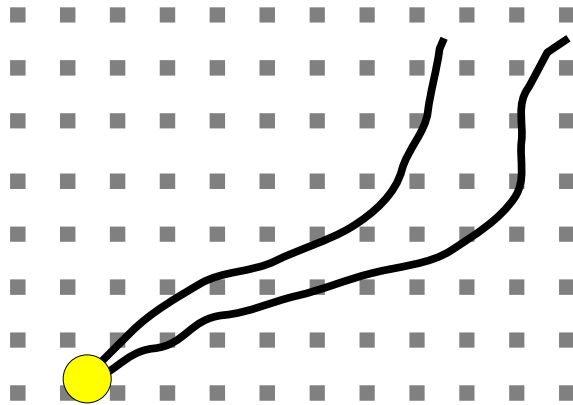
independent estimation



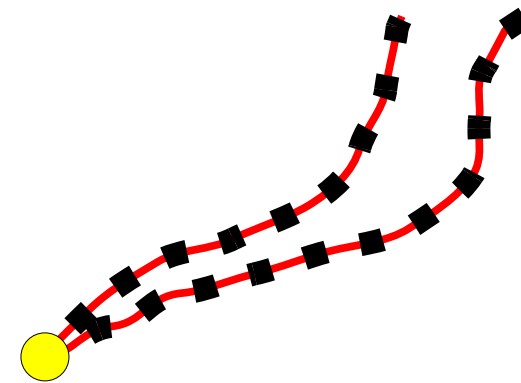
the system: a fiber



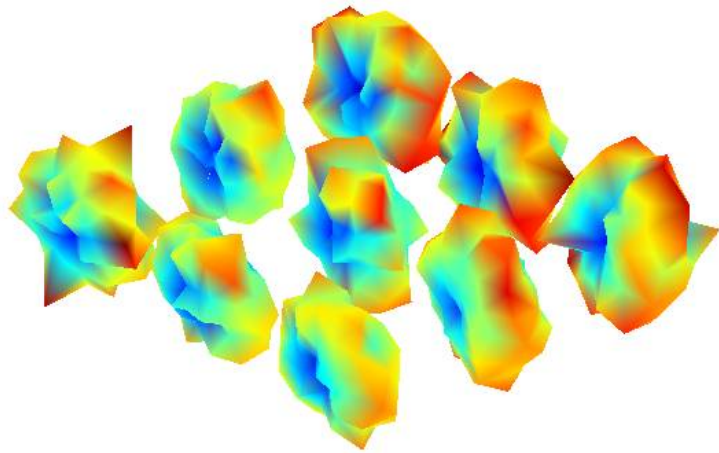
**independent
process**



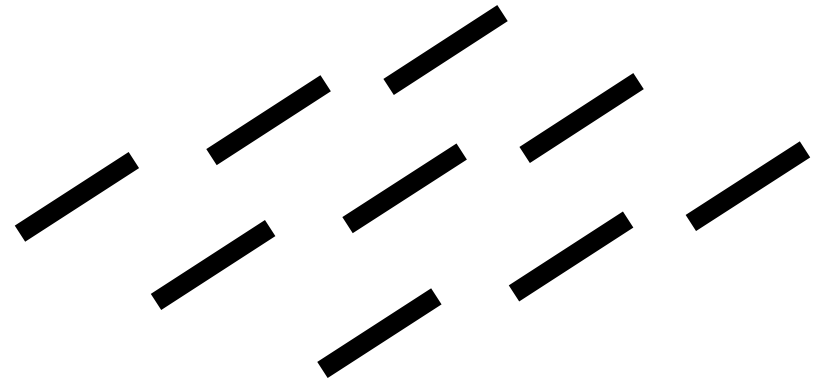
**causal
process**



model-based filtering



scanner measurement



underlying model

objectives:

- estimate model from measurements
- suppress noise

notation

$\mathbf{x}_t$ state of system at time t
state = “model parameters”

$\mathbf{y}_t$ what you see at time t
observation, measurement

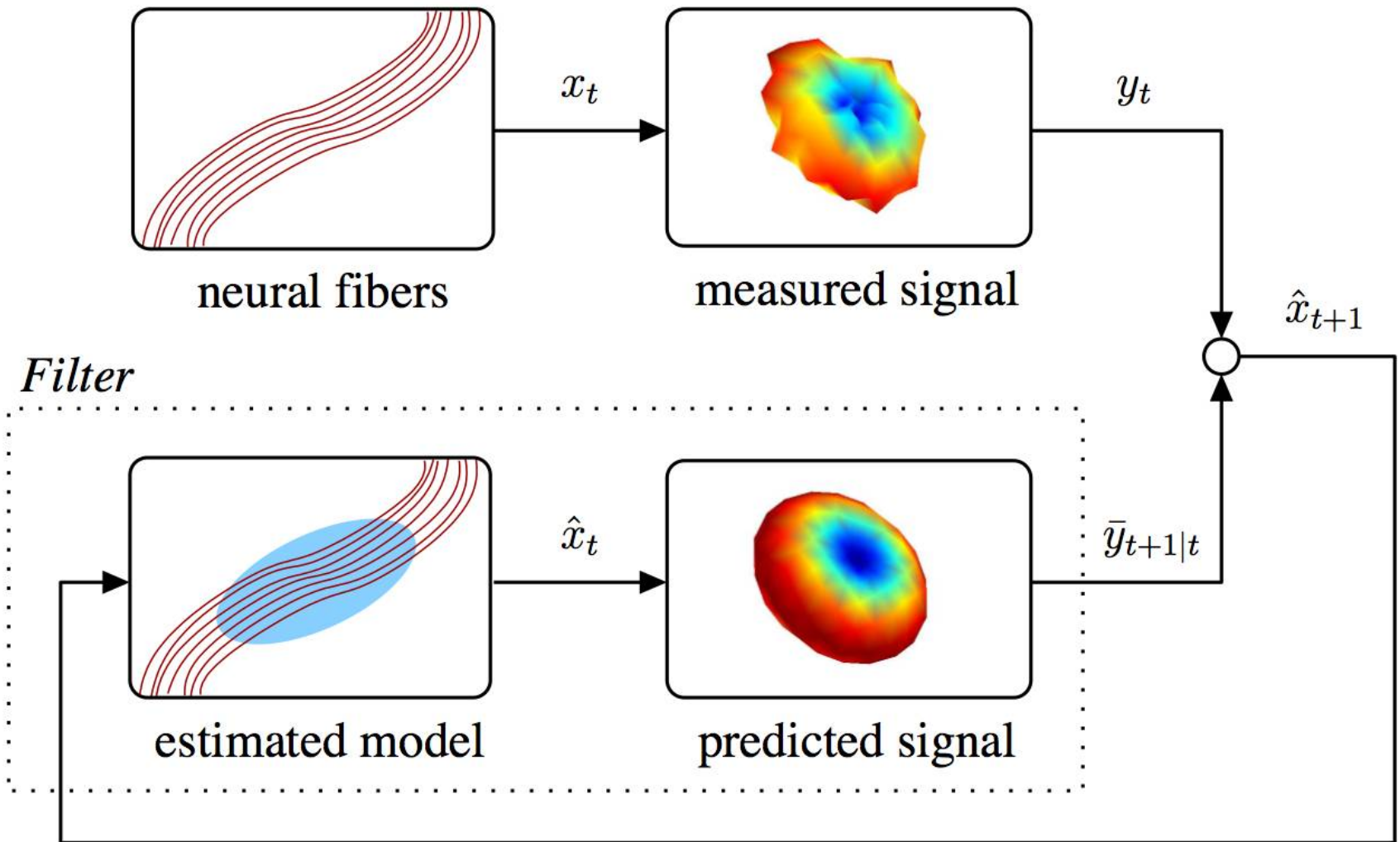
update: $\mathbf{x}_{t+1} = F \mathbf{x}_t$ $\mathbf{x}_{t+1} = f(\mathbf{x}_t)$

observation: $\mathbf{y}_t = G \mathbf{x}_t$ $\mathbf{y}_t = g(\mathbf{x}_t)$

linear

nonlinear

Kalman filtering



predict ... measure ... reconcile ... repeat ...

$$\mathbf{x} = [\mathbf{m}_1 \lambda_{11} \lambda_{12} \mathbf{m}_2 \lambda_{21} \lambda_{22}]^T \in R^{10}$$

10 dimensional state

$\mathbf{y} \in \mathbb{R}^m$ signal

$$\mathbf{x} = [\mathbf{m}_1 \lambda_{11} \lambda_{12} \mathbf{m}_2 \lambda_{21} \lambda_{22}]^T \in R^{10}$$

10 dimensional
state

$$\mathbf{y} \in R^m \text{ signal}$$

$$\mathbf{x}_{t+1} = f(\mathbf{x}_t) = \mathbf{x}_t$$

small steps
slowly varying state

$$\mathbf{y}_t = g(\mathbf{x}_t) = S(\mathbf{u})$$

$$\mathbf{x} = [\mathbf{m}_1 \lambda_{11} \lambda_{12} \mathbf{m}_2 \lambda_{21} \lambda_{22}]^T \in R^{10}$$

$$\mathbf{y} \in R^m \quad \text{signal} \quad \begin{array}{l} 10 \text{ dimensional} \\ \text{state} \end{array}$$

$$\mathbf{x}_{t+1} = f(\mathbf{x}_t) = \mathbf{x}_t \quad \begin{array}{l} \text{small steps} \\ \text{slowly varying state} \end{array}$$

$$\mathbf{y}_t = g(\mathbf{x}_t) = S(\mathbf{u})$$

$$y(\mathbf{u}) = S(\mathbf{u}) = 0.5 s_0 e^{-b \mathbf{u}^T D_1 \mathbf{u}} + 0.5 s_0 e^{-b \mathbf{u}^T D_2 \mathbf{u}}$$

$$D = \lambda_1 \mathbf{m} \mathbf{m}^T + \lambda_2 (\mathbf{p} \mathbf{p}^T + \mathbf{q} \mathbf{q}^T)$$

signal reconstruction is nonlinear

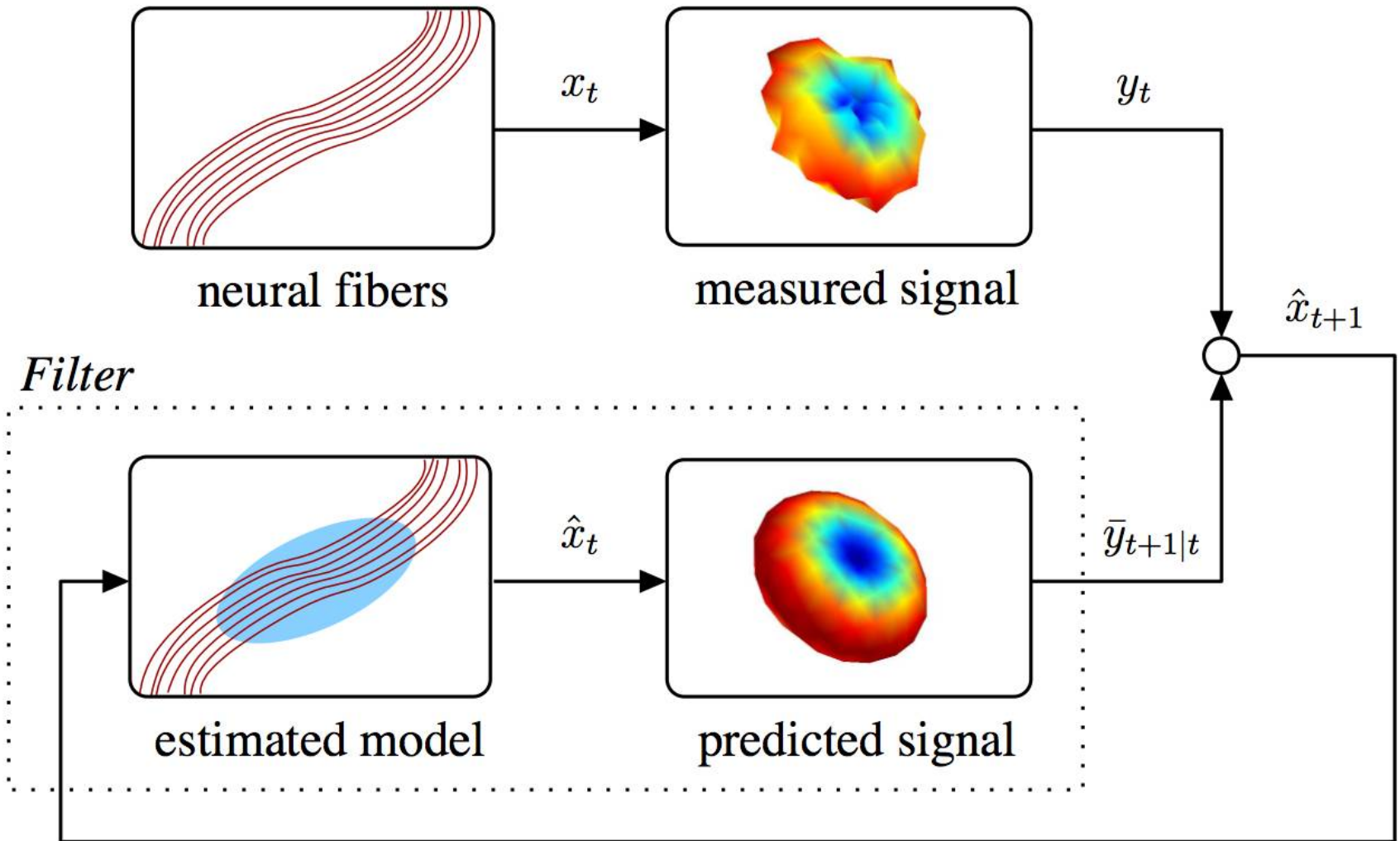
independent optimization

- least squares
linearization
- gradient descent
local minima
- Levenberg-Marquardt
local minima

causal estimation

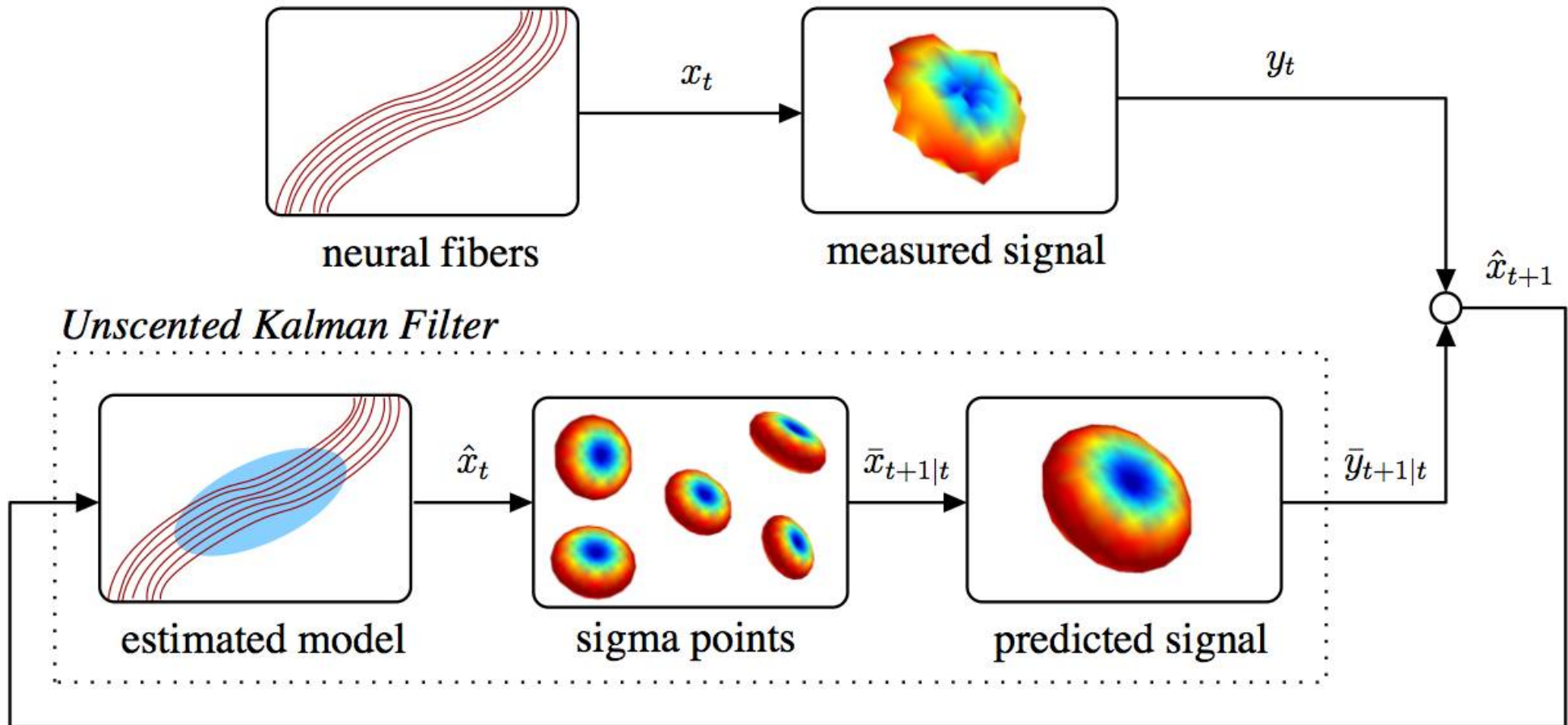
- extended Kalman filter
mean + covariance
linearization
- particle filter
non-parametric
sampling
- unscented Kalman filter
mean + covariance
no linearization
limited sampling

linear Kalman filter



predict ... measure ... reconcile ... repeat ...

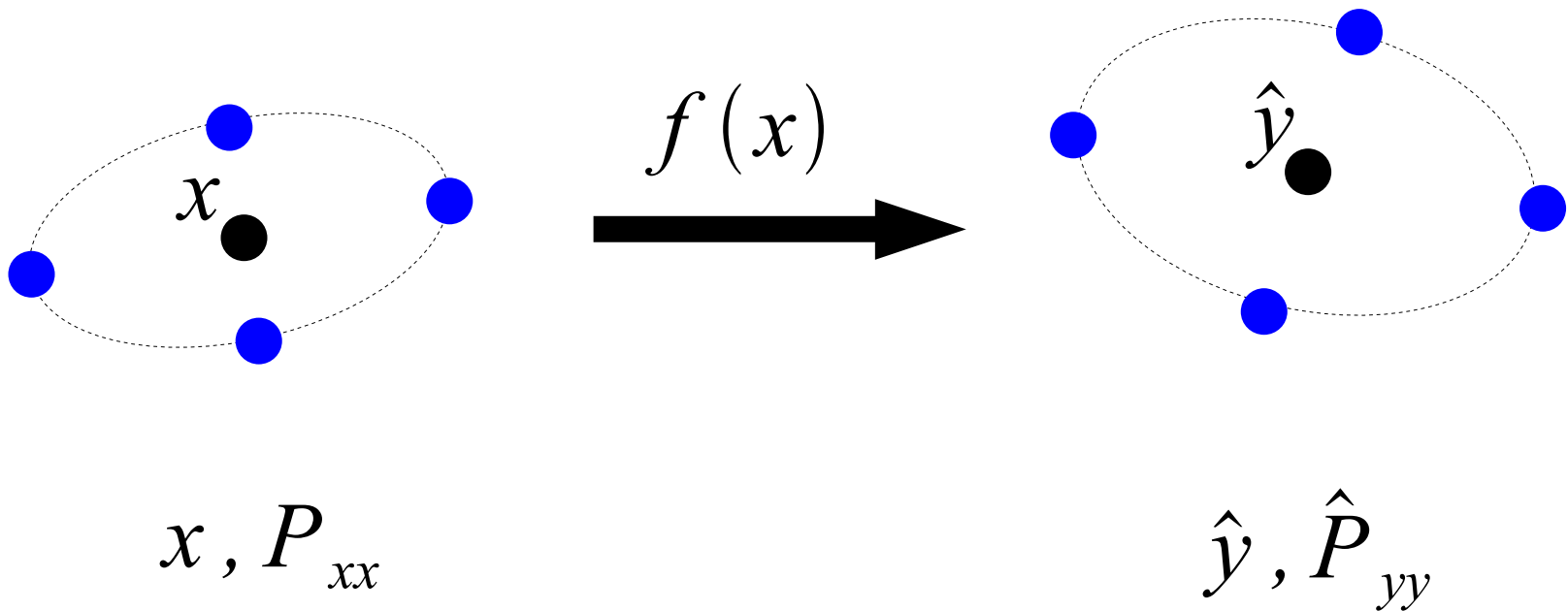
unscented Kalman filter



same update equations
modified prediction step

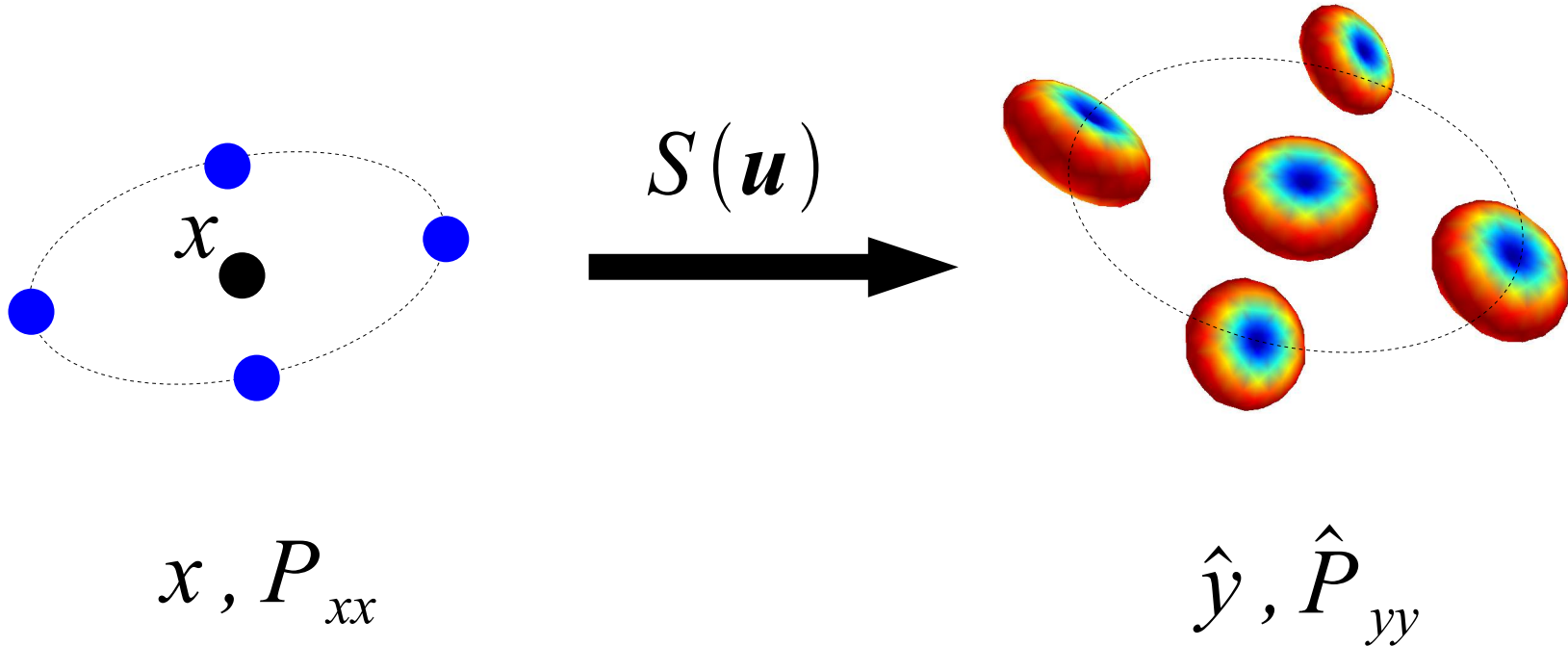
unscented transform

approximate the statistics...not the function



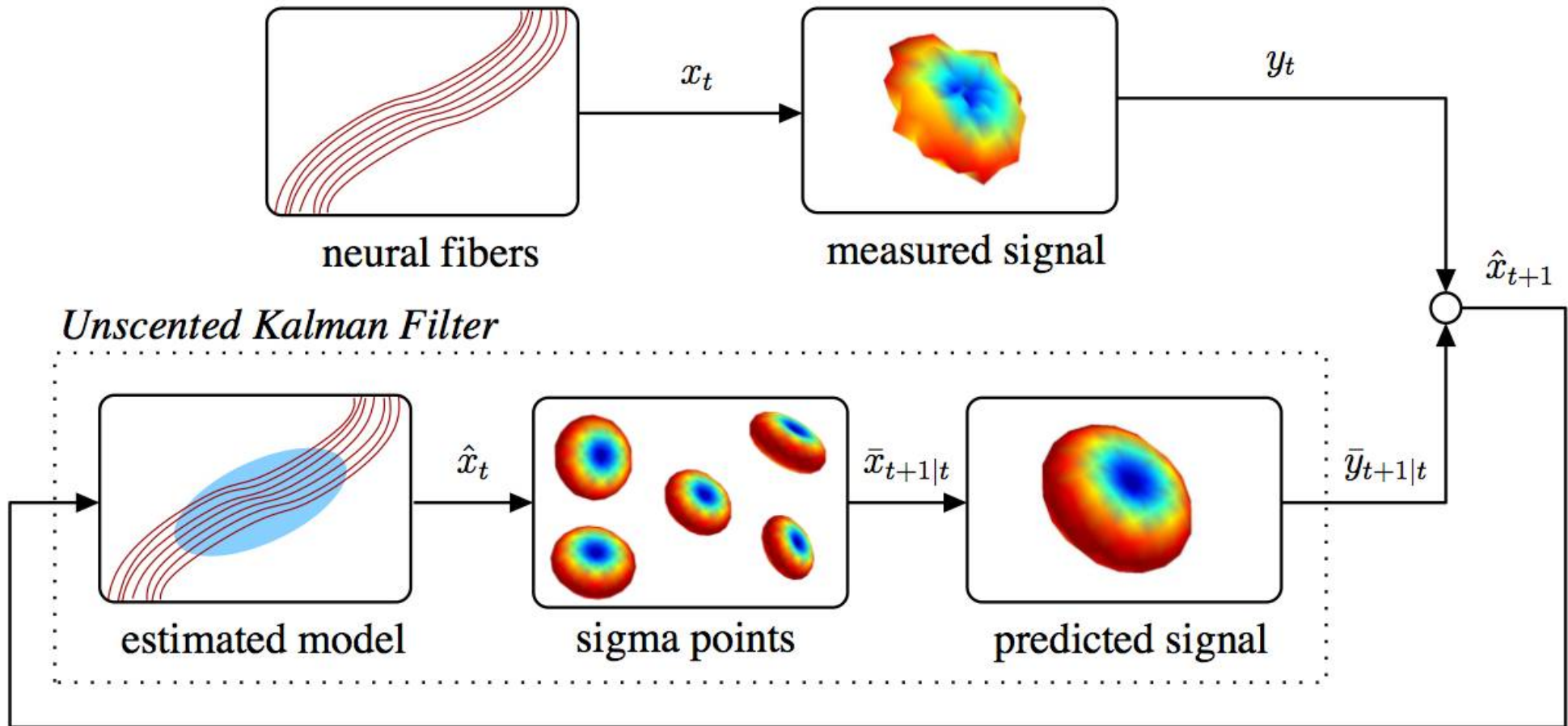
unscented transform

for signal reconstruction...



$$x = [\mathbf{m}_1 \lambda_{11} \lambda_{12} \mathbf{m}_2 \lambda_{21} \lambda_{22}]^T$$

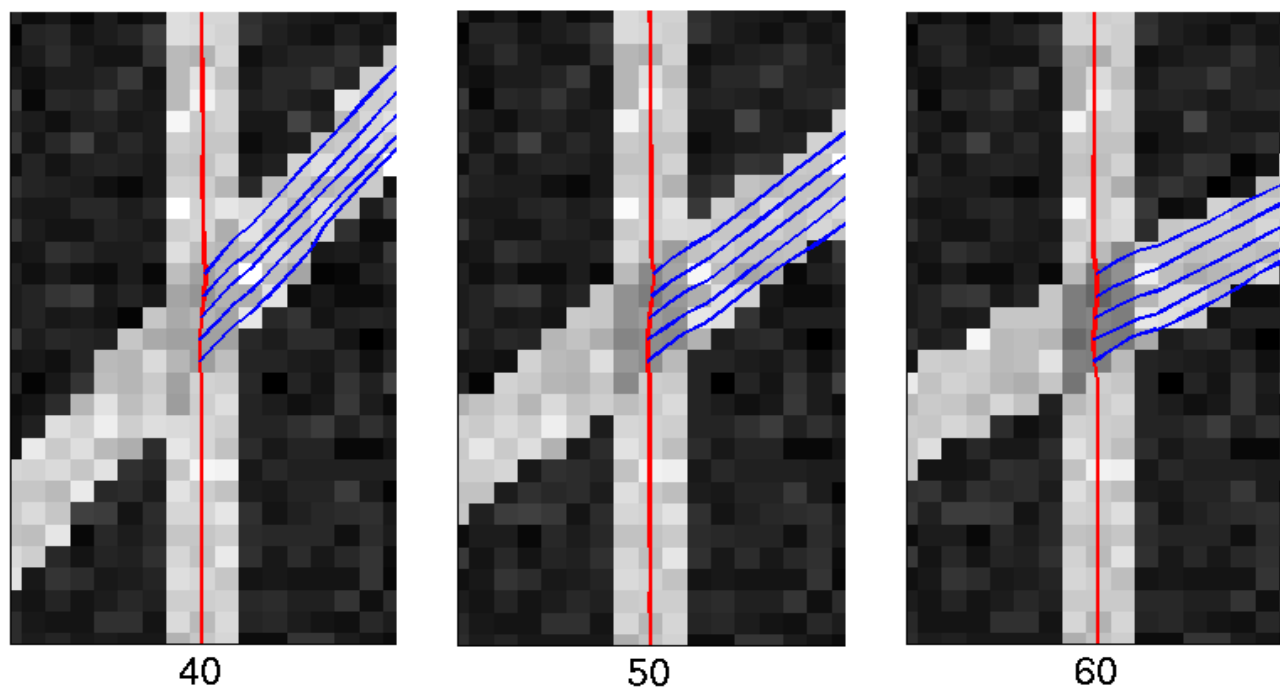
unscented Kalman filter



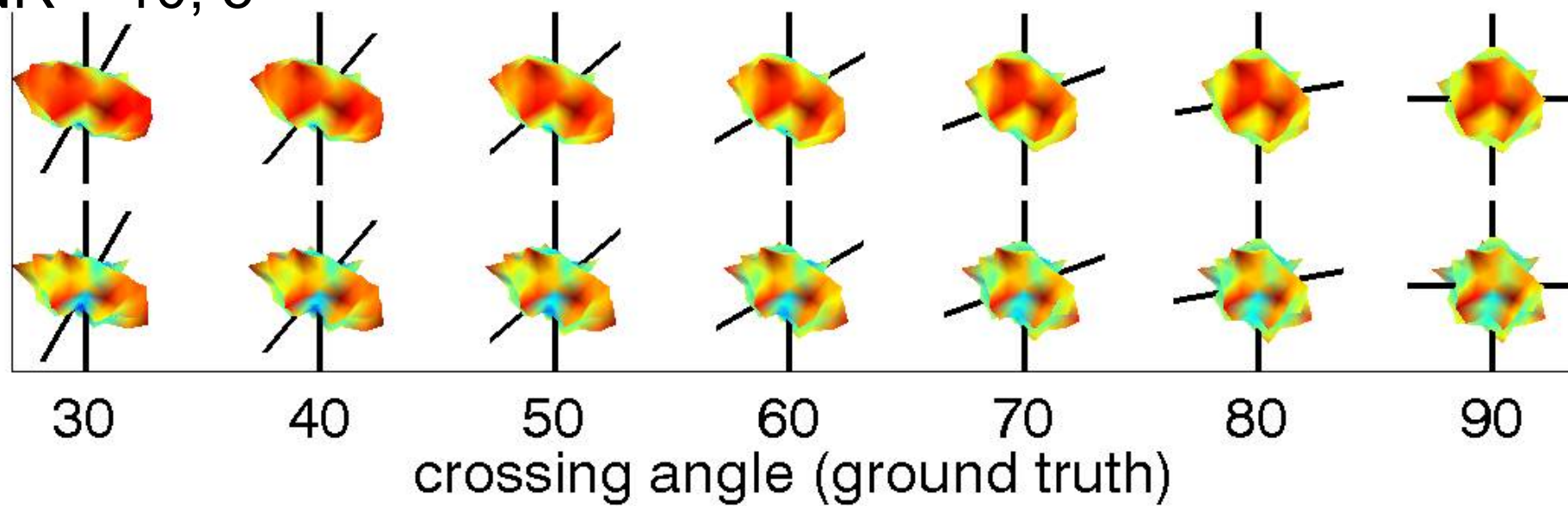
predict ... measure ... reconcile ... repeat ...

synthetic validation

$b = 1000$



SNR $\approx 10, 5$



brute force optimization

- matching pursuit
- parametric dictionary
- noiseless signal
- discretization, noise

spherical harmonics

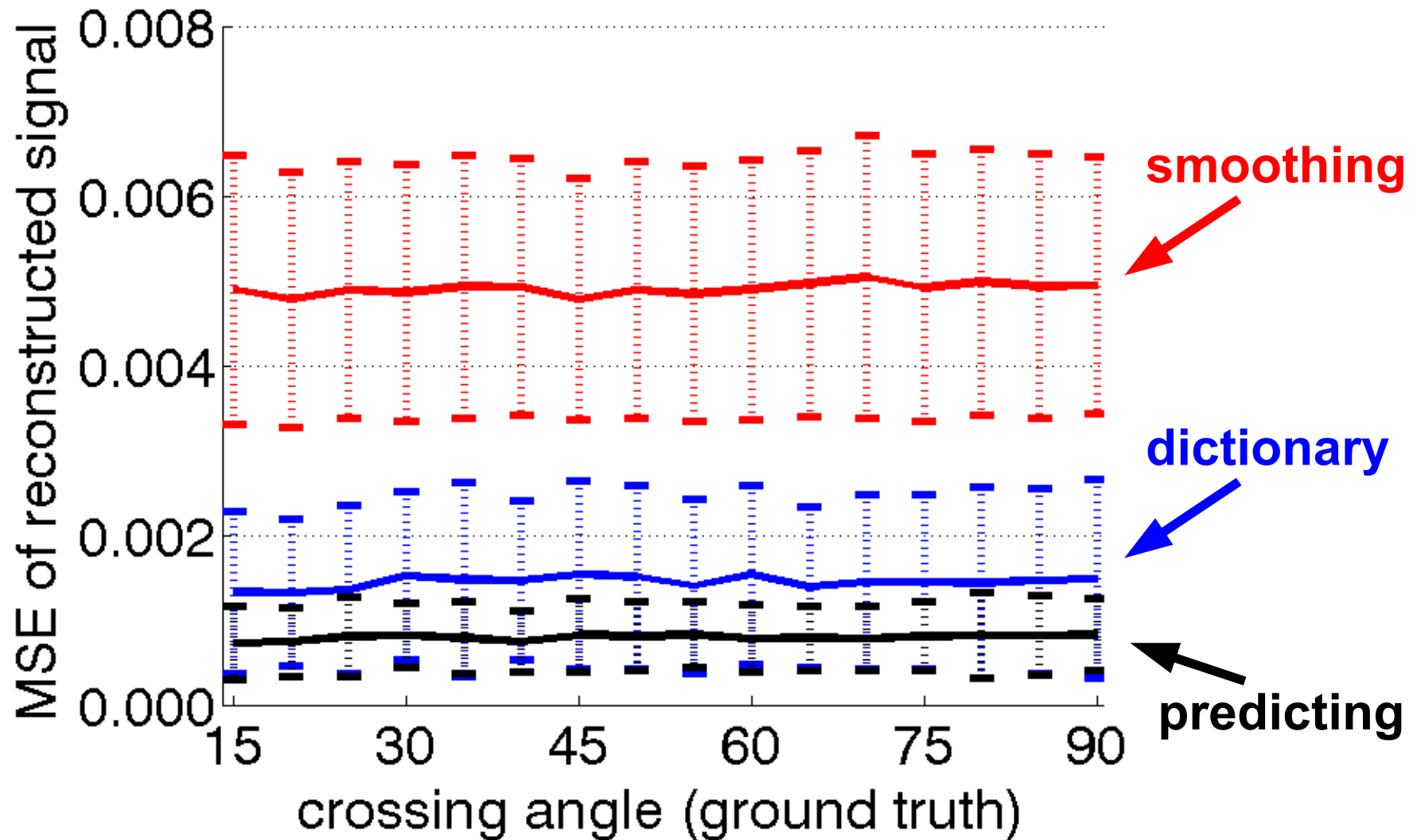
- non-parametric
- order eight (8)
- fiber sharpening for peak detection ($L=0.006$)

[Descoteaux 07]

filtered tractography

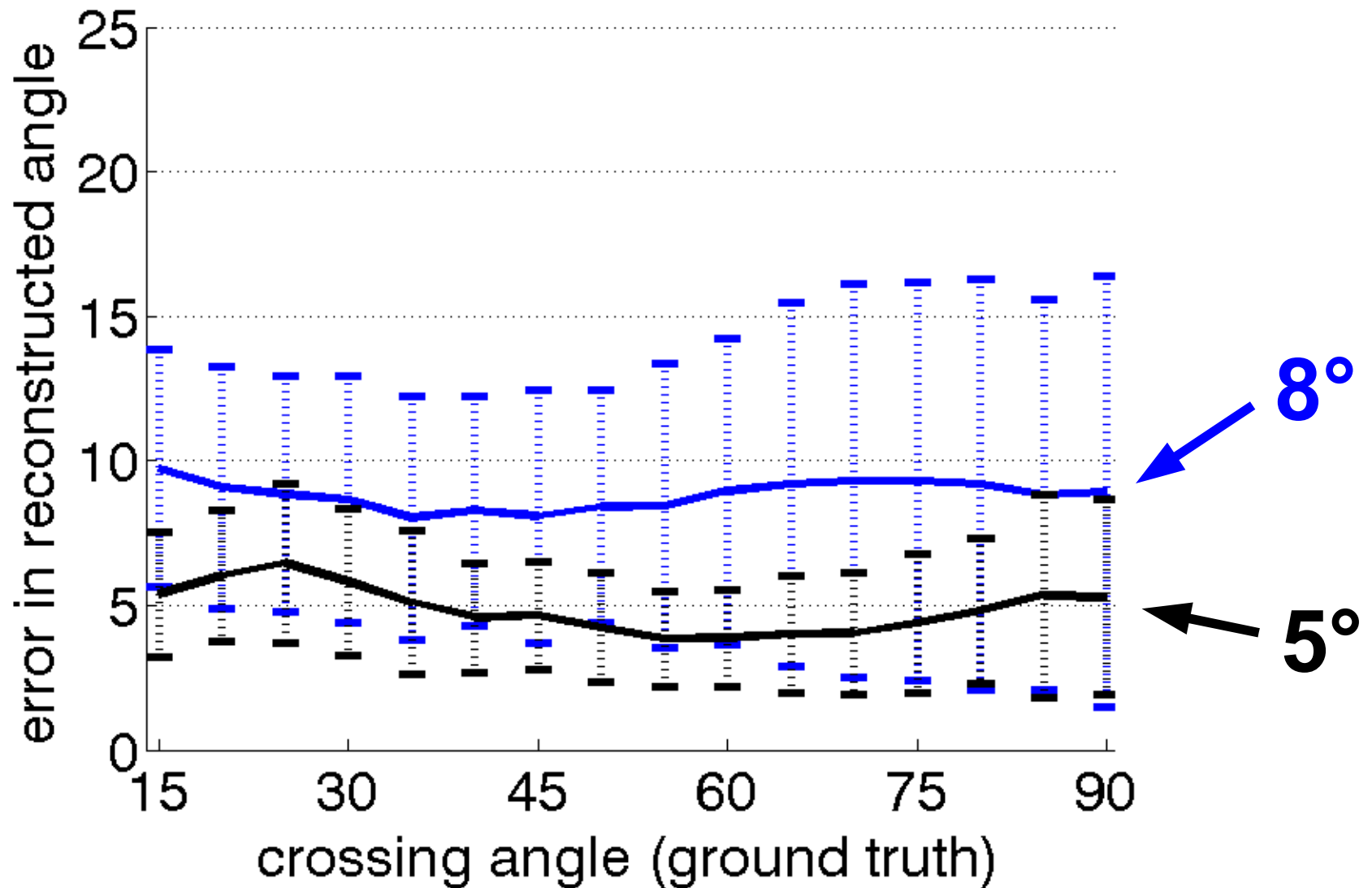
- two-fiber model
- unscented Kalman filter

signal reconstruction error



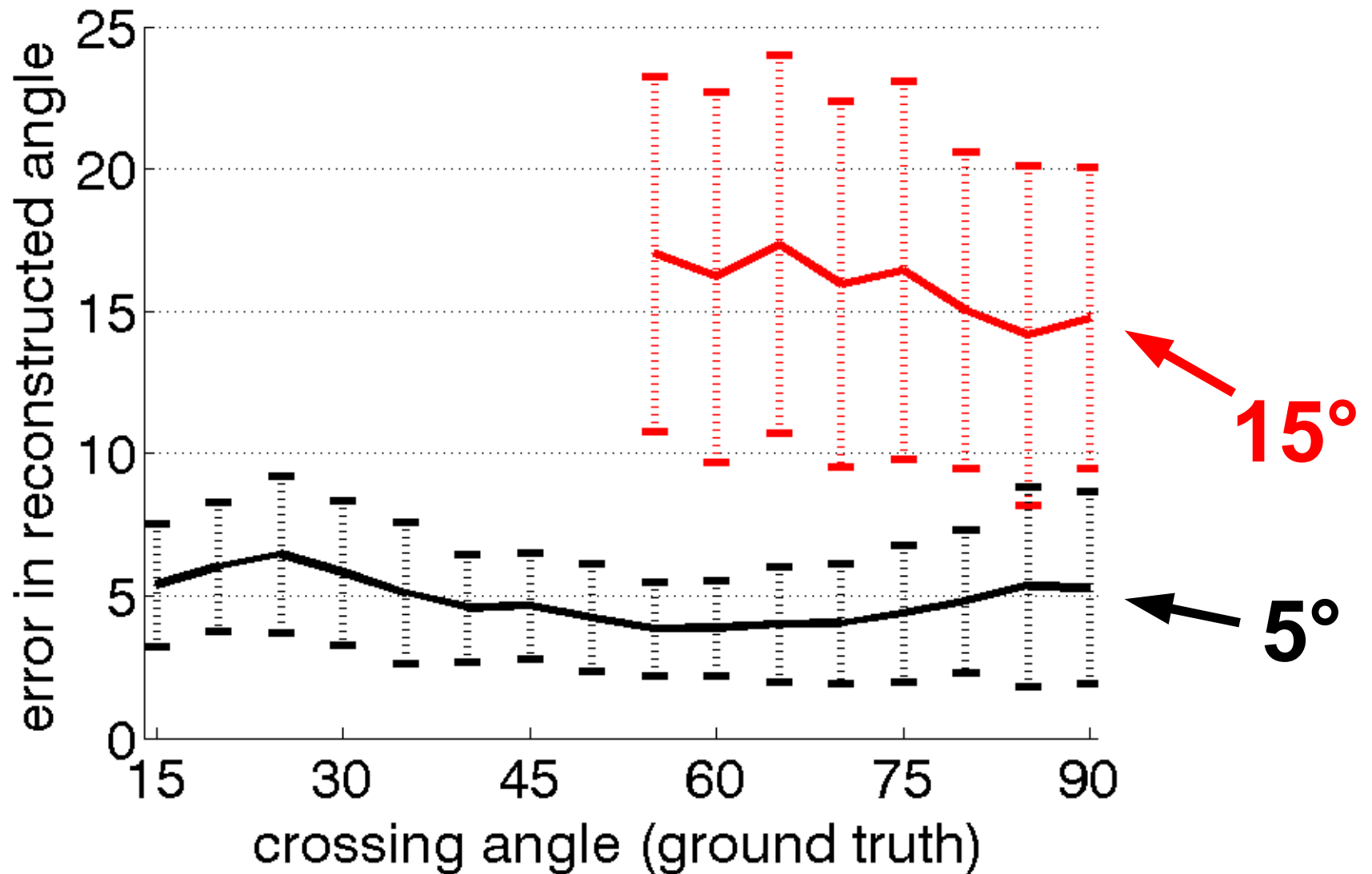
SNR ≈ 5 , $b = 1000$

angular reconstruction error



SNR ≈ 5 , $b = 1000$

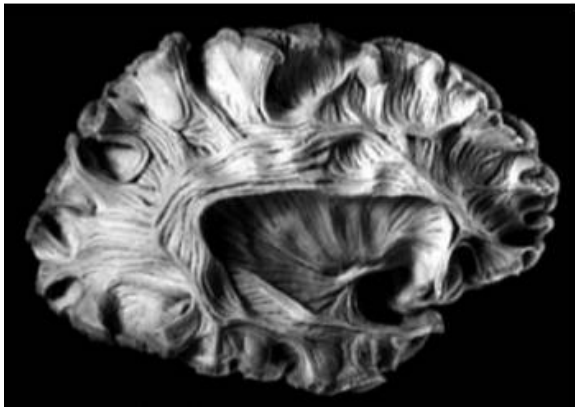
angular reconstruction error



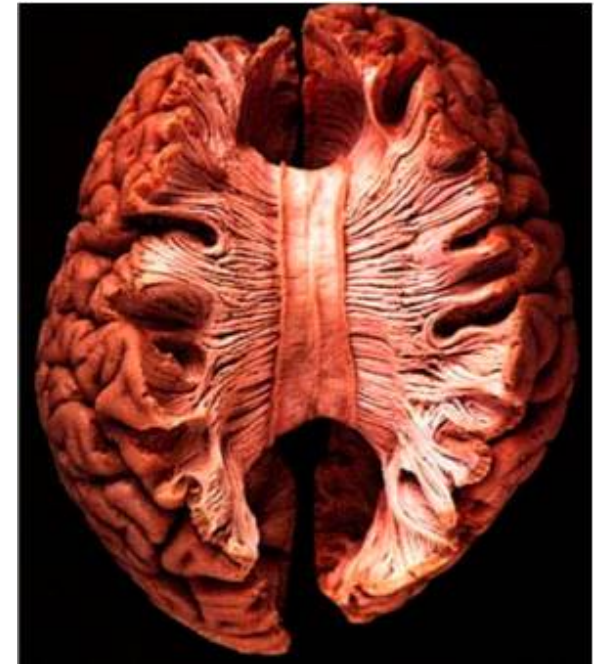
SNR ≈ 5 , $b = 1000$



in vivo



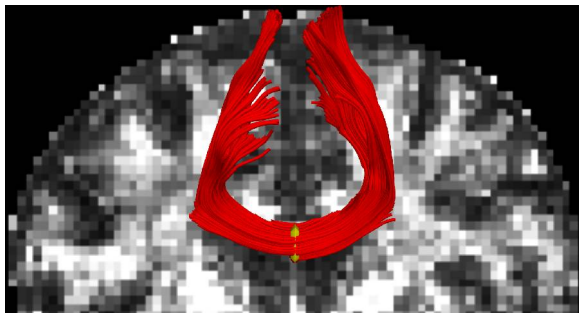
b=900
51 directions
1.7mm isotropic voxel
17 minute scan



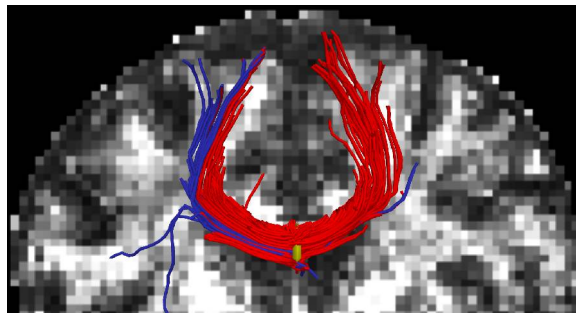
algorithm

- 1)interpolate scanner signal (measurement)
- 2)estimate model parameters with UKF
- 3)proceed in most consistent direction
- 4)repeat

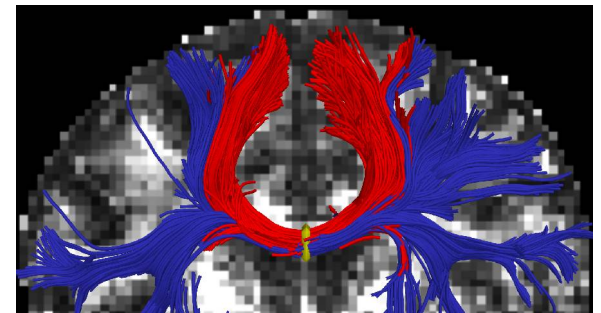
- branch: $\theta < 40^\circ$
- terminate: $FA < 0.15$ or $GA < 0.10$



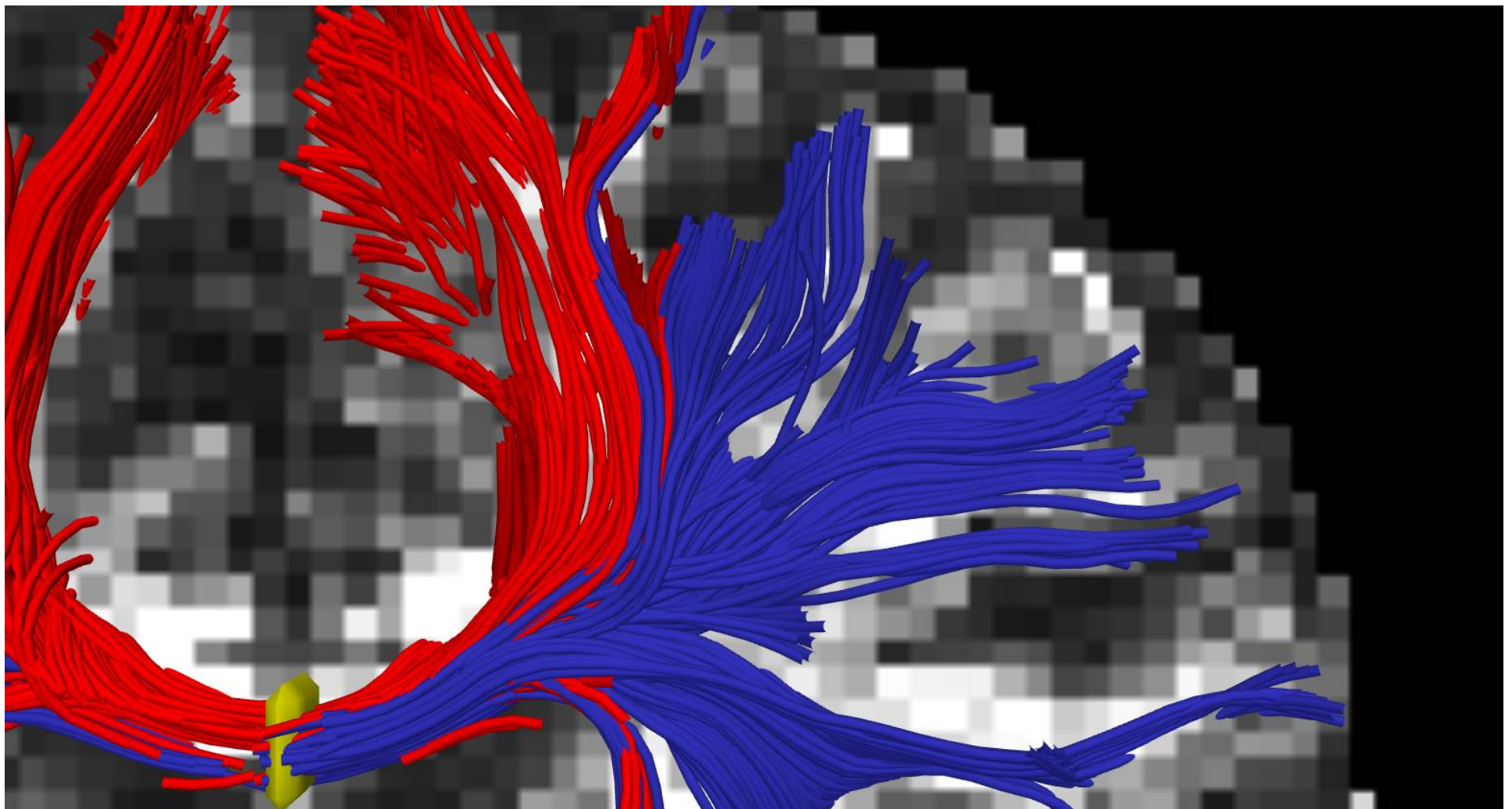
single tensor



spherical harmonics

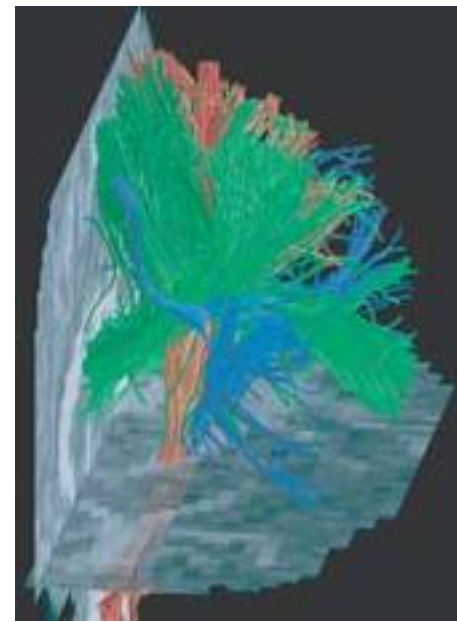
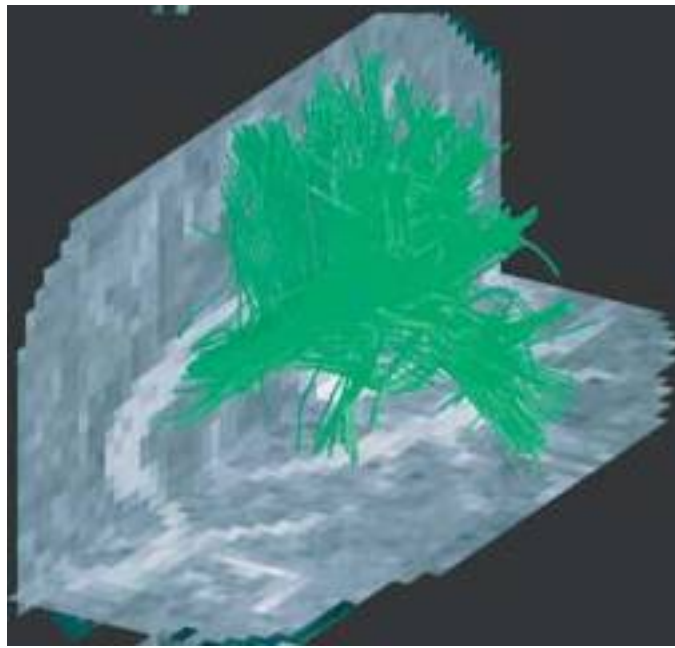


filtered two-tensor

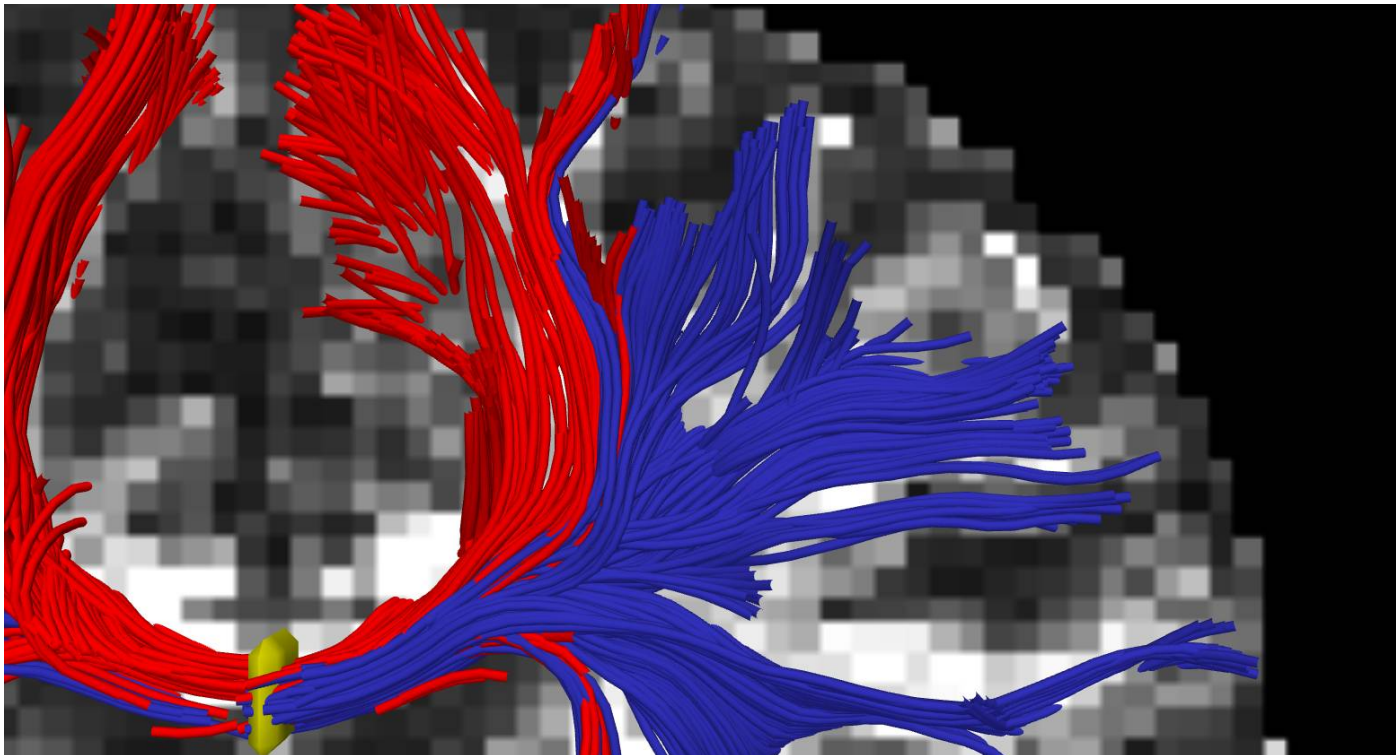


filtered two-tensor

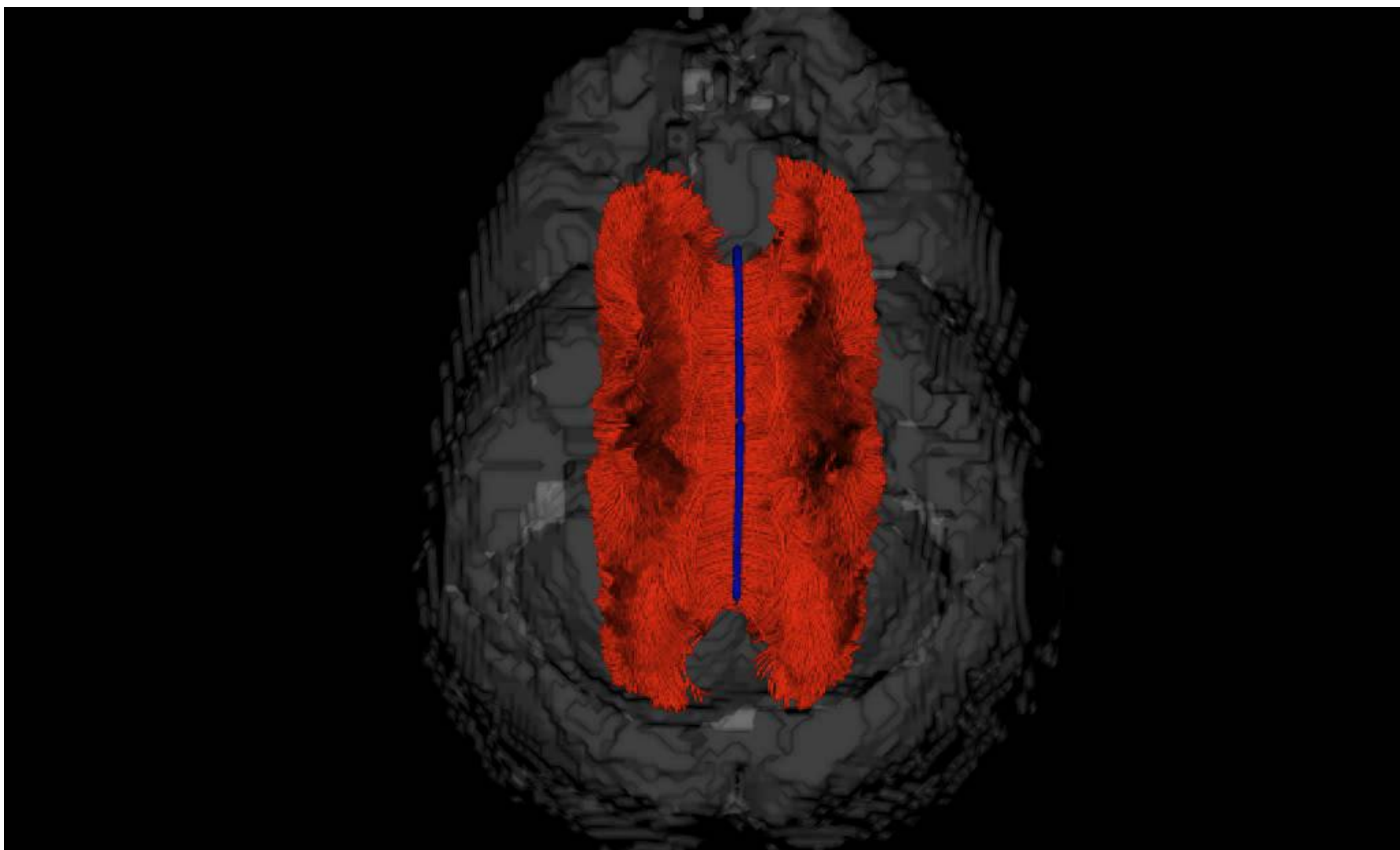
(b = 900, 1.7mm, 51 directions)

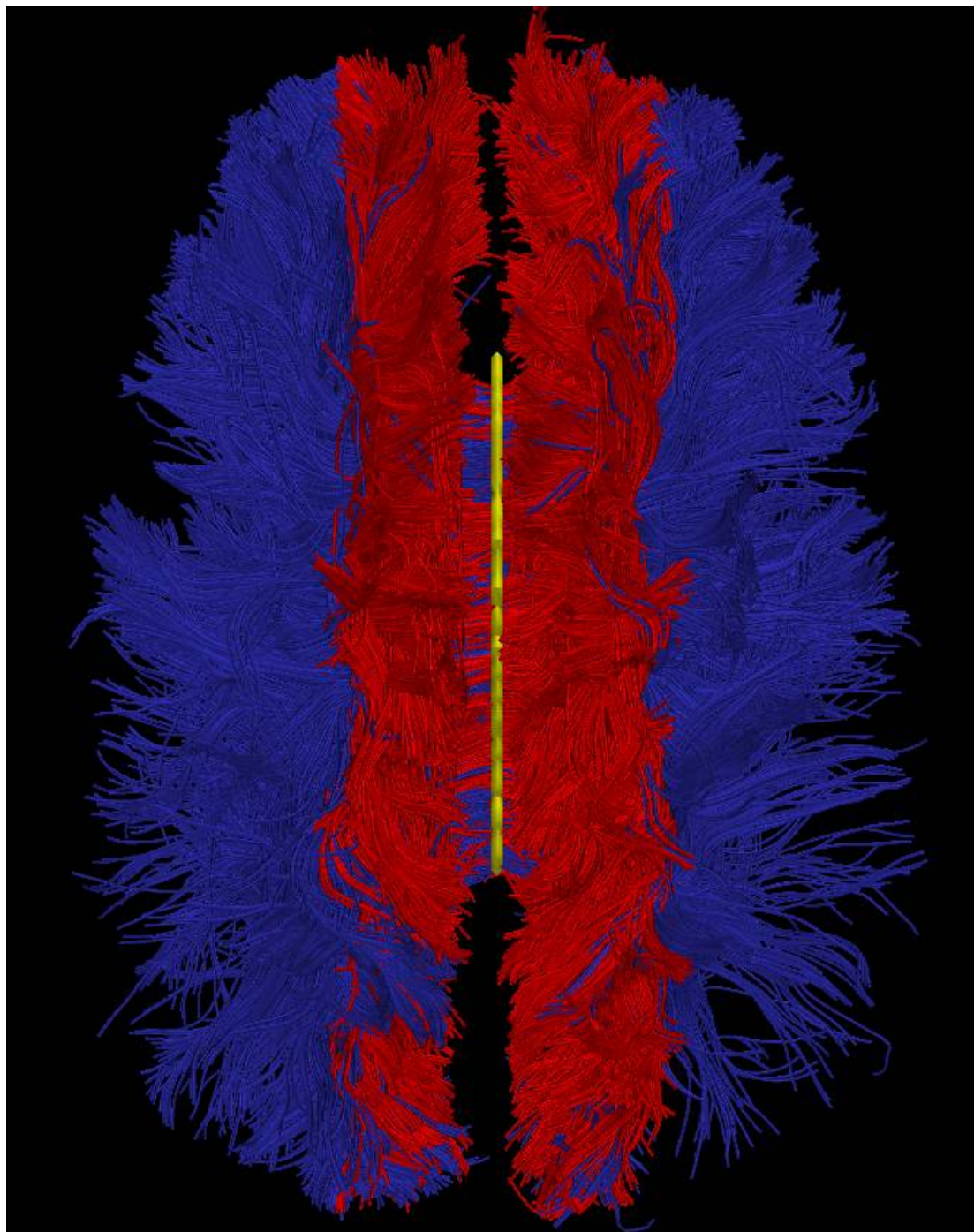


DSI [Hagmann 05]



filtered two-tensor

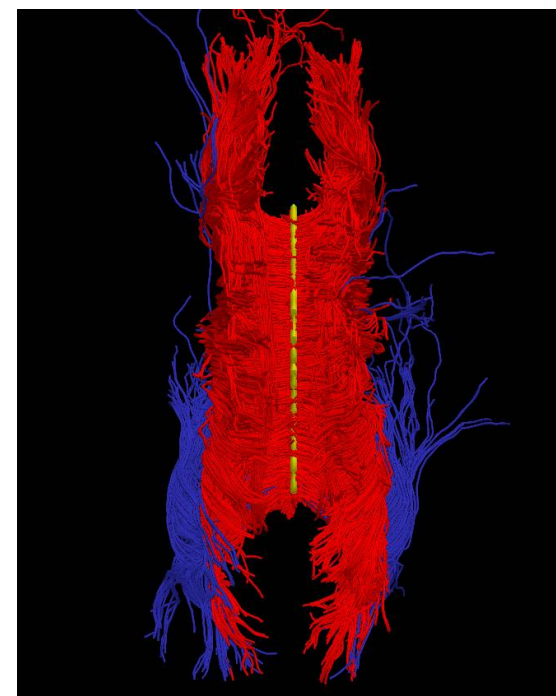




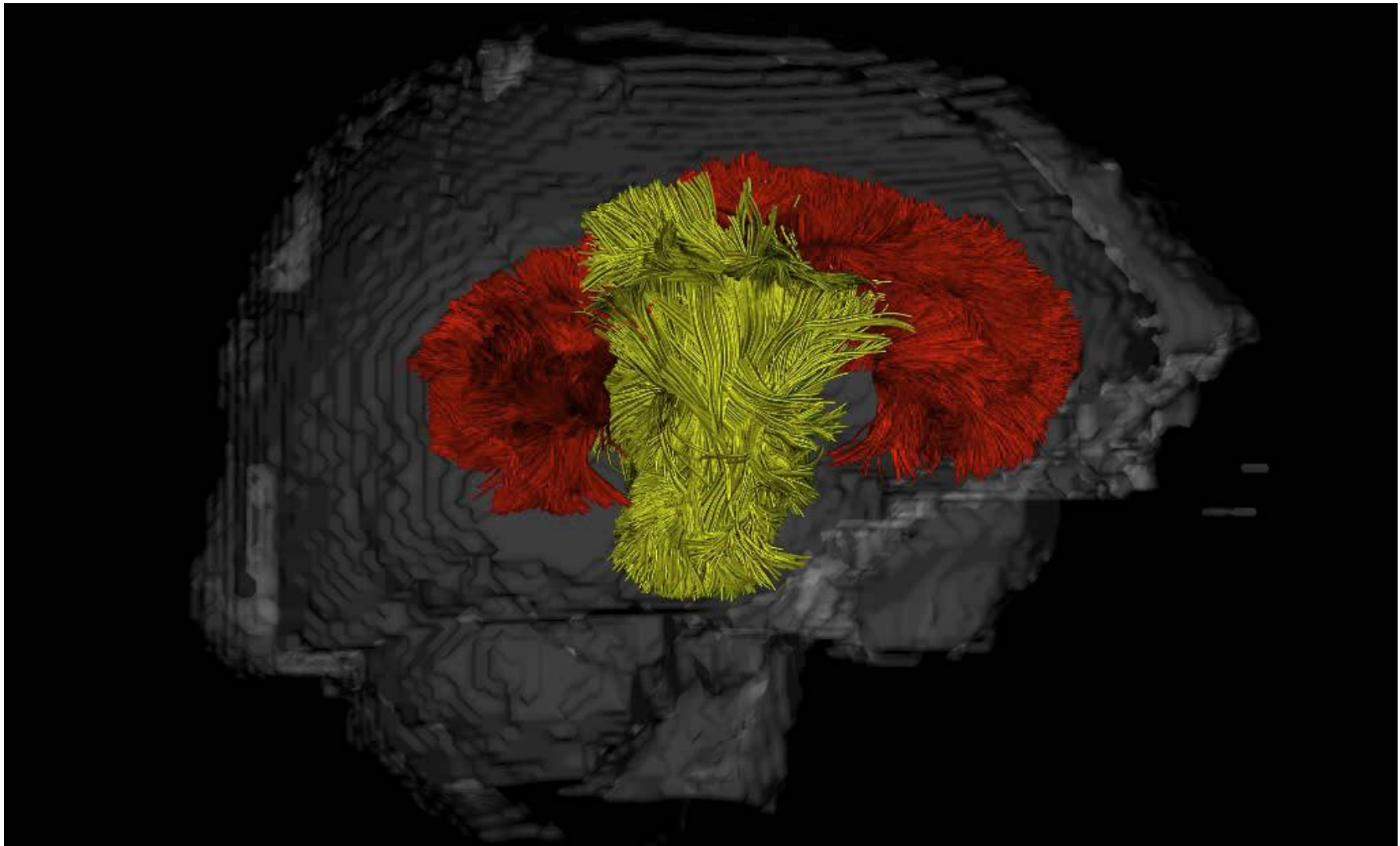
filtered two-tensor



single tensor

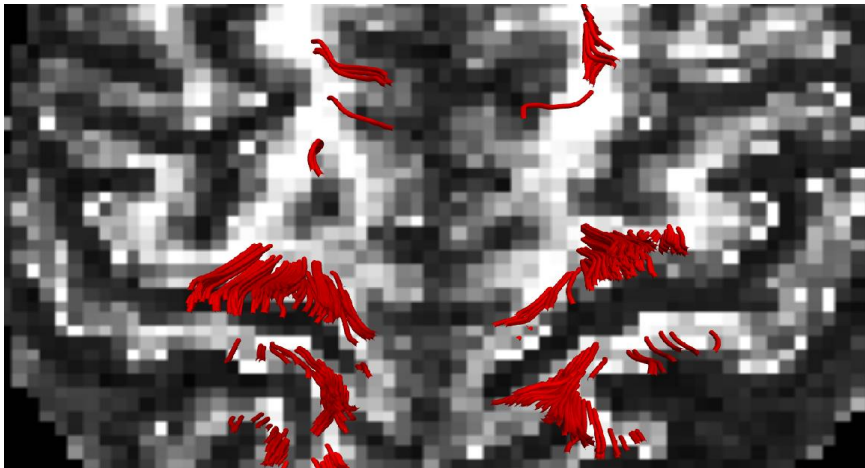


spherical harmonics

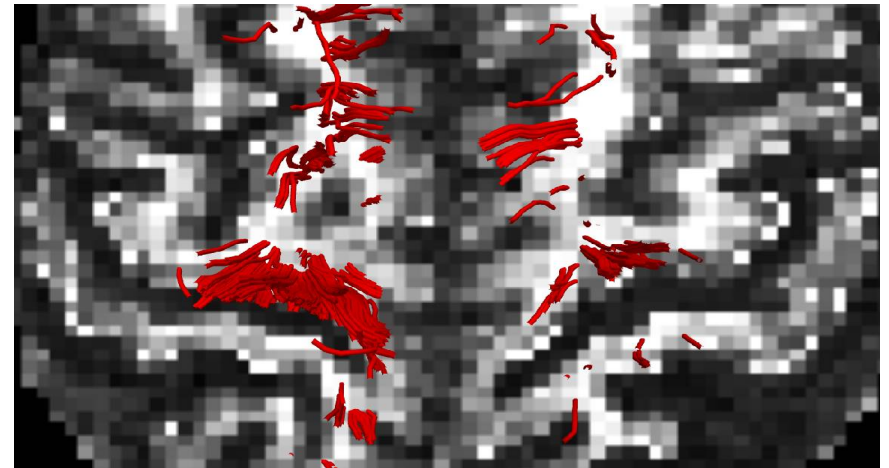


corpus callosum

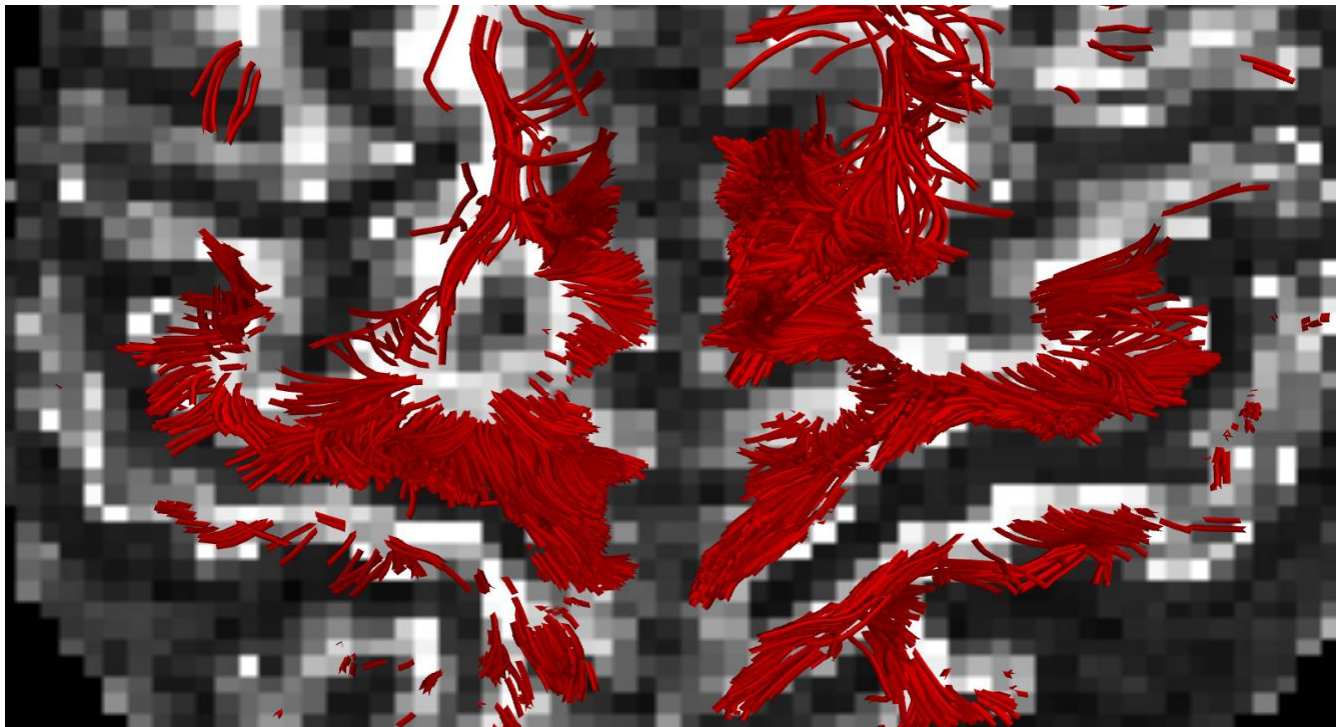
internal capsule



single tensor



spherical harmonics



filtered two-tensor

10°

20°

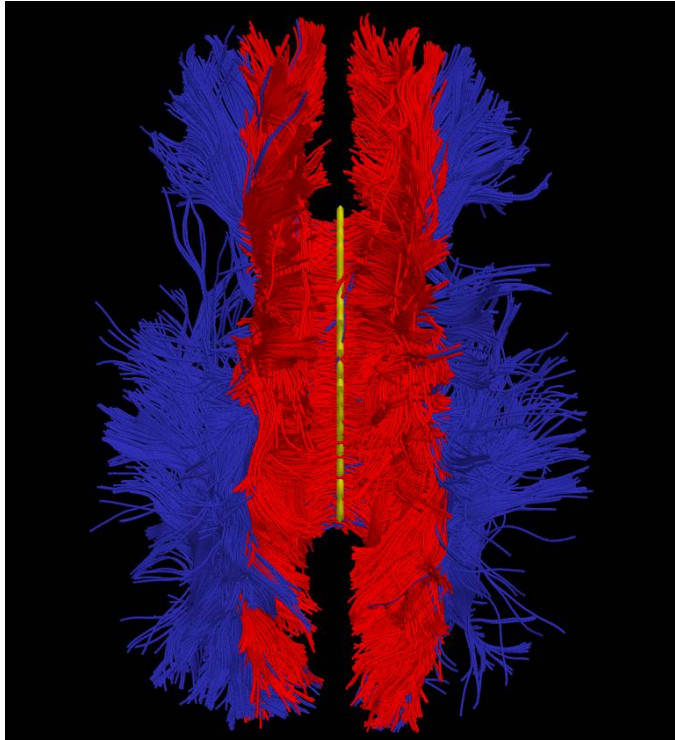
30°

40°

primary

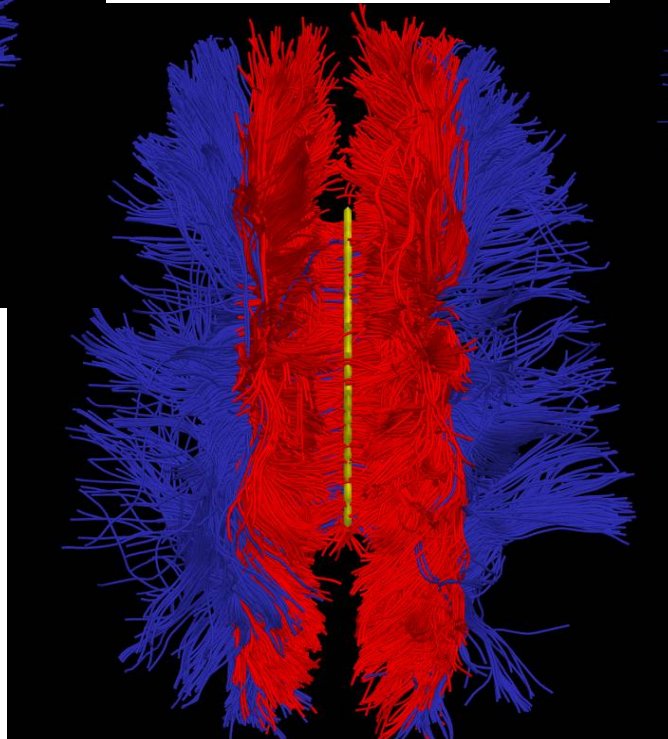
branches

variations on a theme

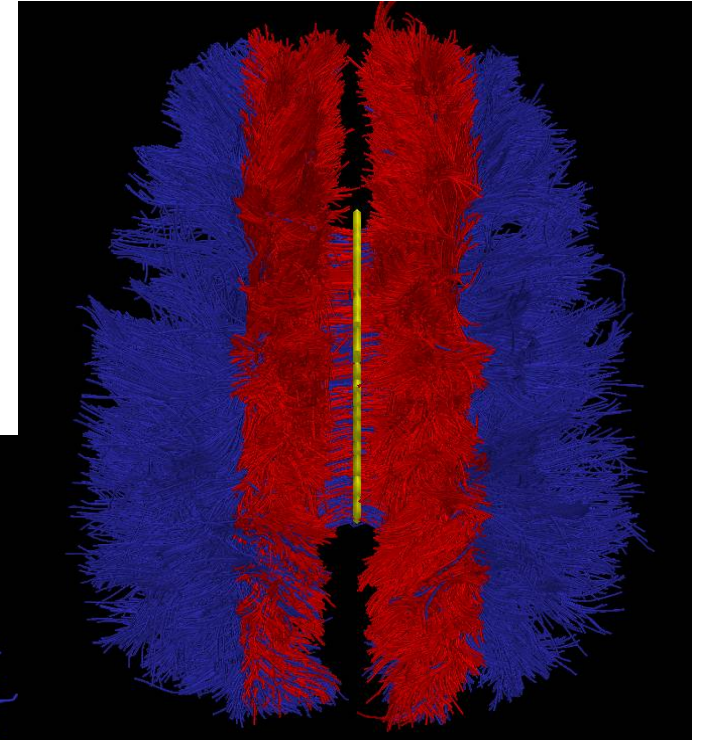


directional functions

parametric:
mixture models
non-parametric:
spherical harmonics
higher-order tensors



weighted models



three tensors

conclusion

inherent coherence along the fiber

we should exploit it in the estimation

discussion

model assumptions

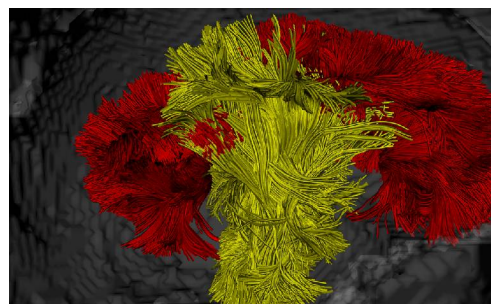
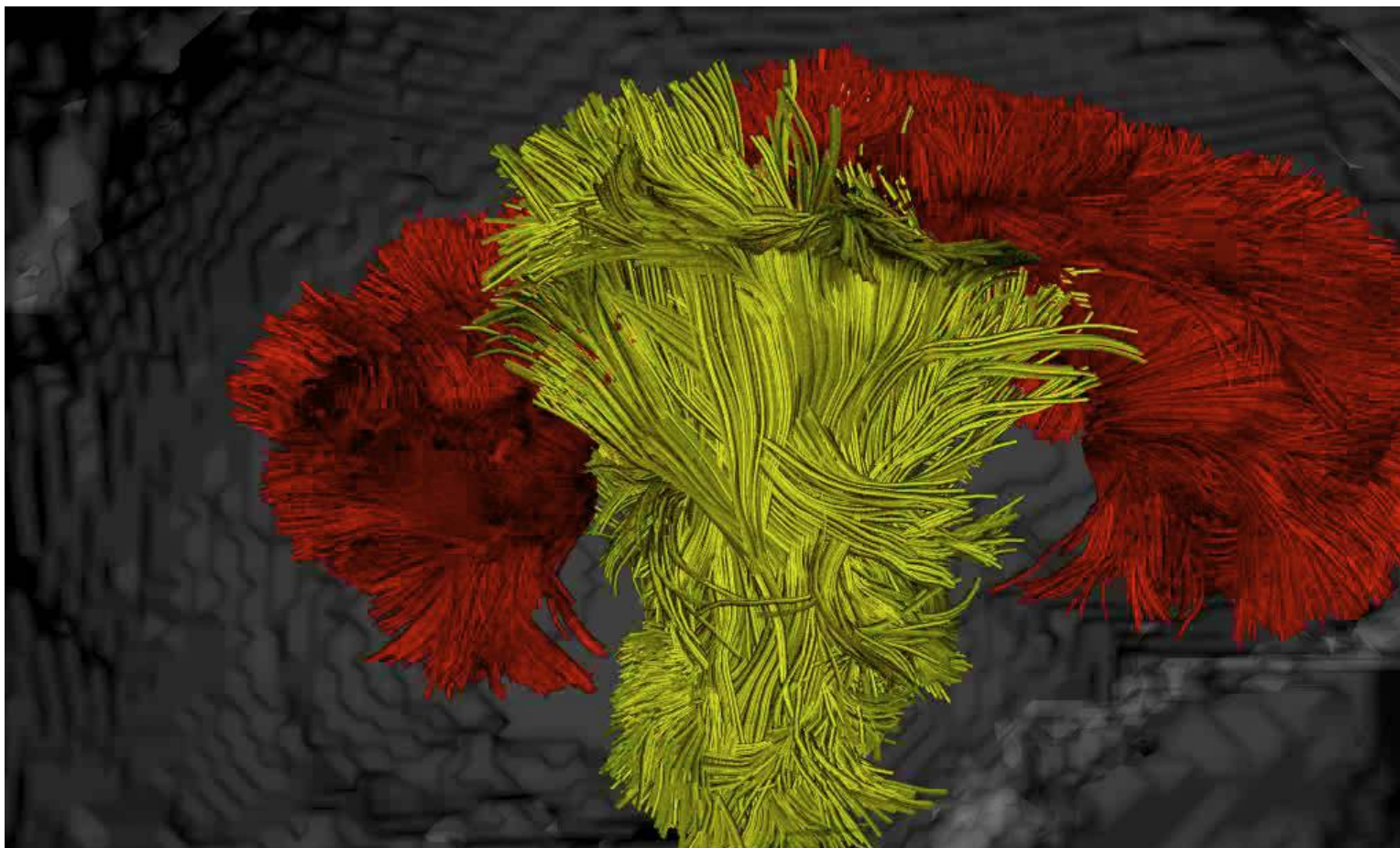
...in this study

Two fibers
single fiber: align

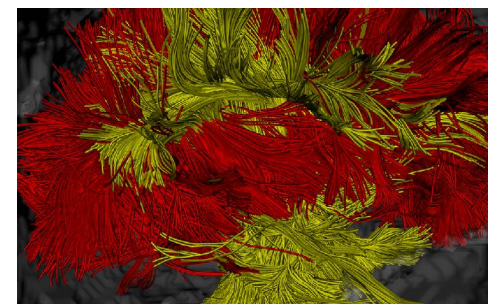
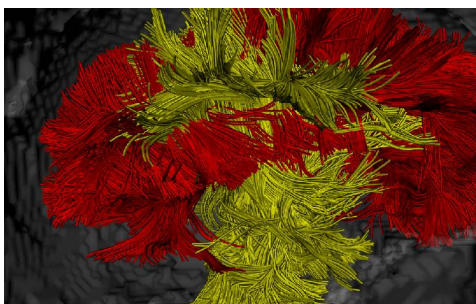
Fixed volume fractions
eigenvalues

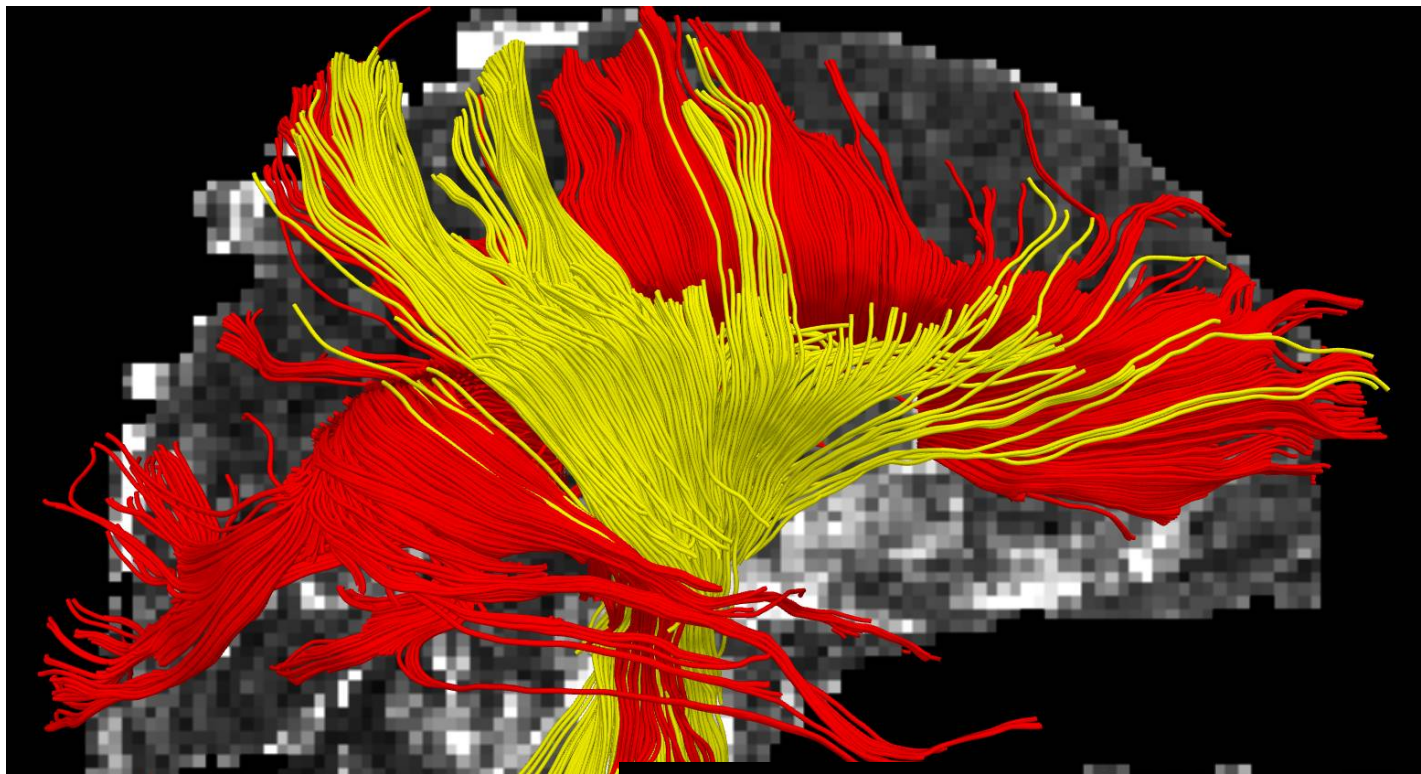
Tensors are elliptic or isotropic
disc ($\lambda_1 = \lambda_2 > \lambda_3$)

model selection, non-parametric, ...



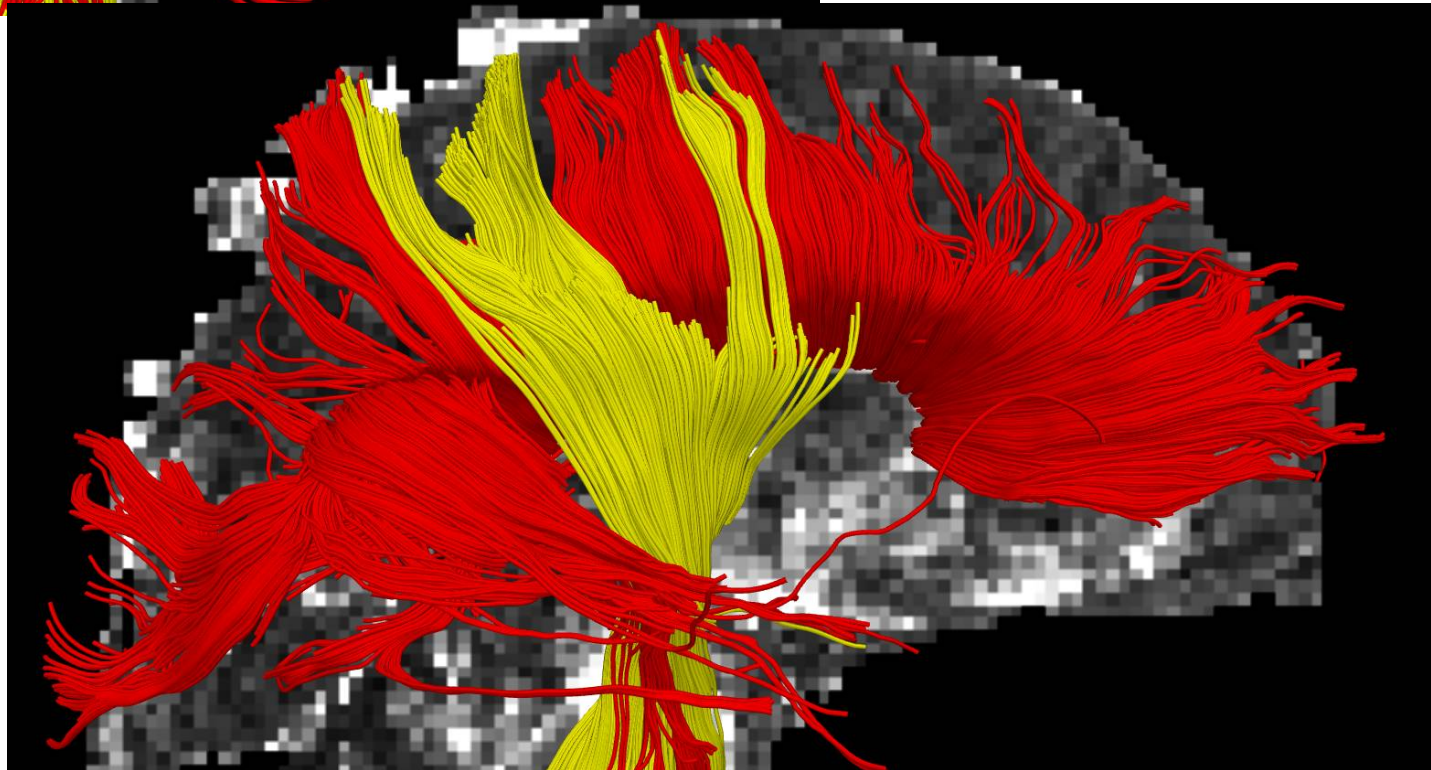
centrum semiovale



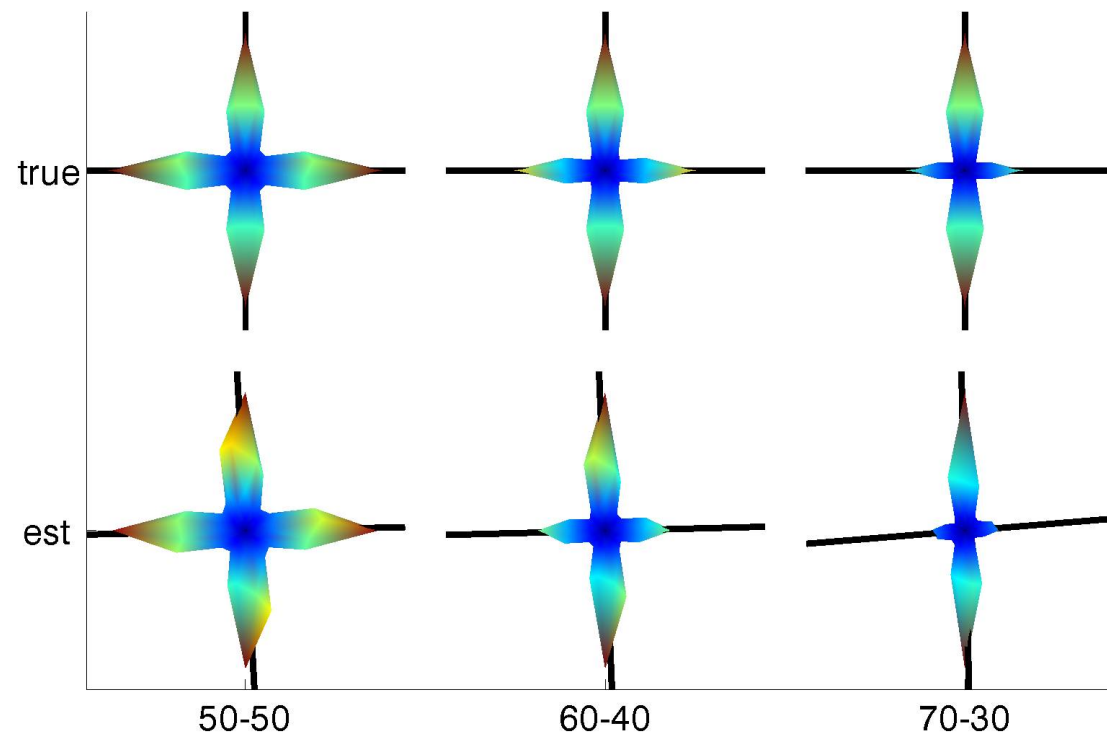


streamline
single-tensor

filtered
single-tensor

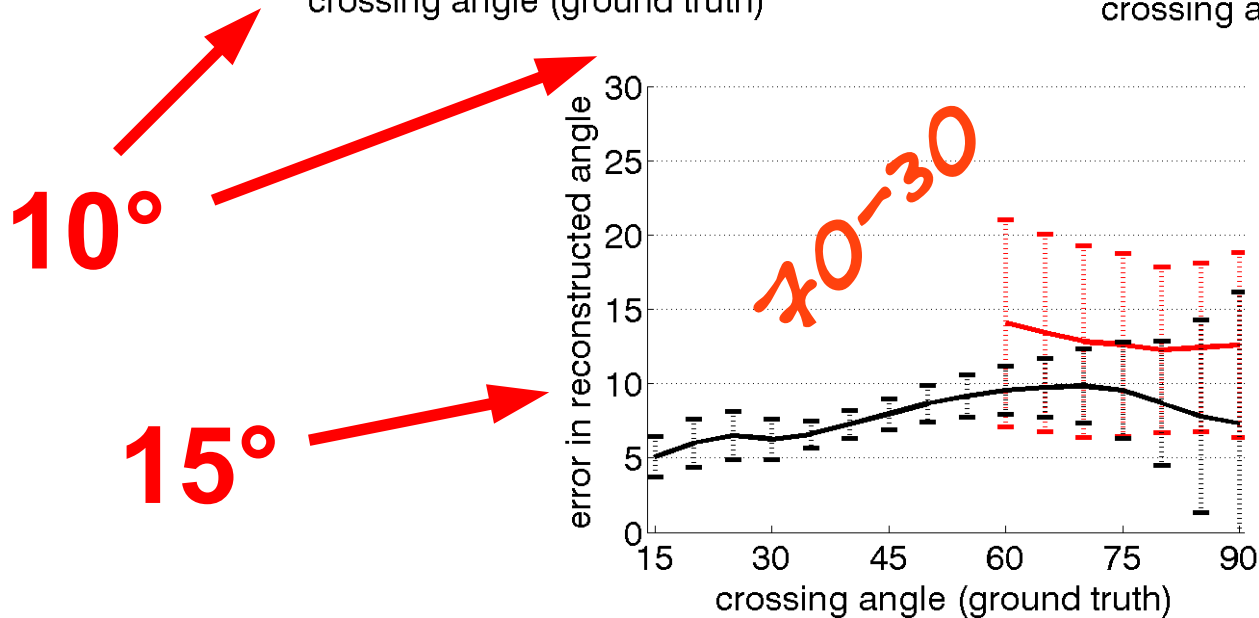
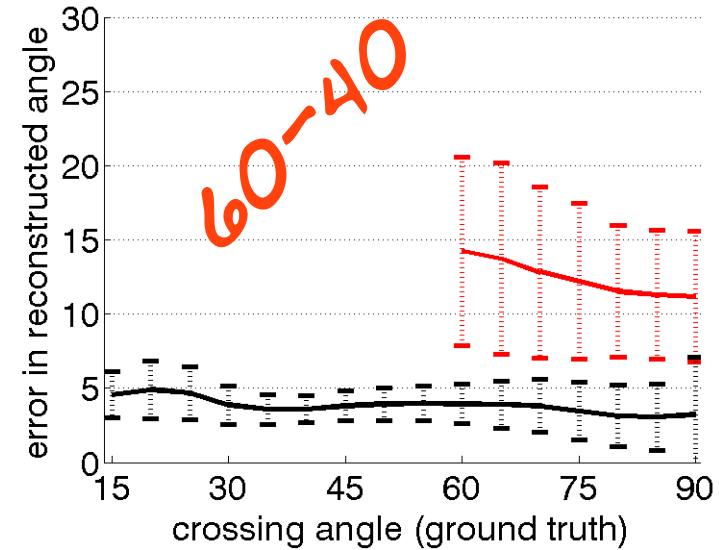
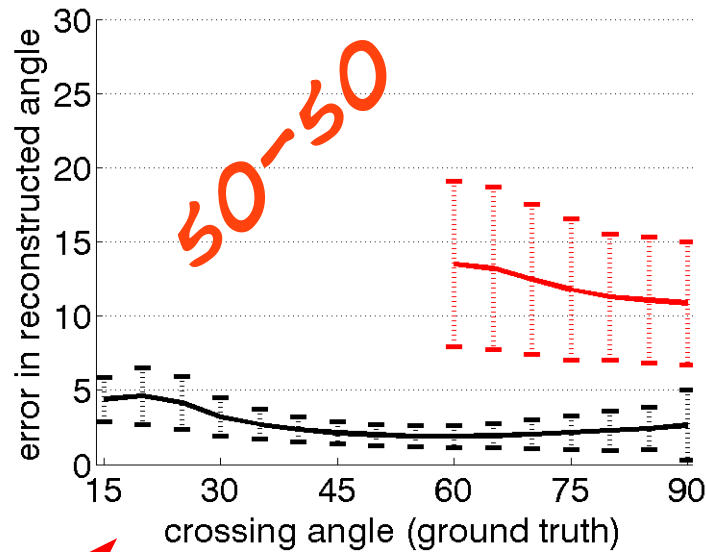


volume fractions



SNR $\approx$ 10, $b = 1000$

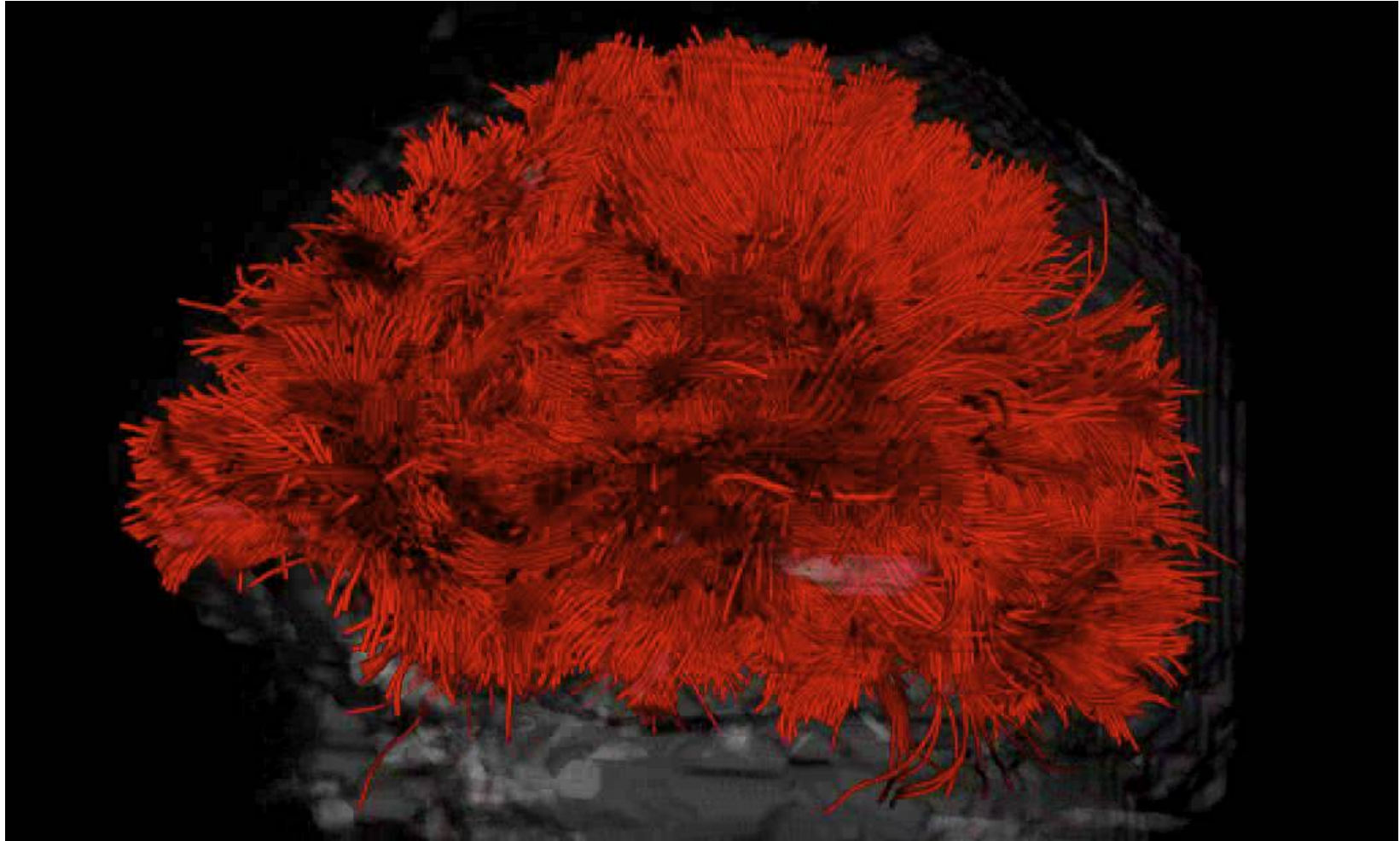
volume fractions



filter
deteriorates

SNR ≈ 10 , $b = 1000$

end



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