

# Filtered Tractography Validation on a Physical Phantom

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*Diffusion Modeling and Fiber Cup*  
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method:  
the model

# multi-tensor mixture model

$$S(\mathbf{u}) = s_0 \sum_j w_j e^{-b \mathbf{u}^T D_j \mathbf{u}}$$

$D_j$  diffusion tensor

$\mathbf{u}$  unit

$w_j$  direction  
convex

$b$  weights  
acquisition

$s_0$  constant  
null signal  
( $b=0$ )

# model assumptions

*...in this project*

Two fibers

Fixed volume fractions

Tensors are elliptic or isotropic

# model parameters

for two fibers...

...two principal directions     $m \in \mathbb{R}^3$

...two primary eigenvalues     $\lambda_1 \in \mathbb{R}$

...two minor eigenvalues     $\lambda_2 \in \mathbb{R}$

5 + 5 = 10 parameters

# model parameters

for two fibers...

...two principal directions  $\mathbf{m} \in \mathbb{R}^3$

...two primary eigenvalues  $\lambda_1 \in \mathbb{R}$

...two minor eigenvalues  $\lambda_2 \in \mathbb{R}$

**5 + 5 = 10 parameters**

$$S(\mathbf{u}) = 0.5 s_0 e^{-b \mathbf{u}^T D_1 \mathbf{u}} + 0.5 s_0 e^{-b \mathbf{u}^T D_2 \mathbf{u}}$$

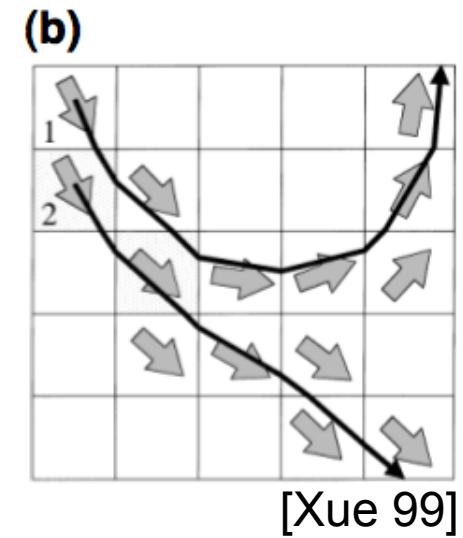
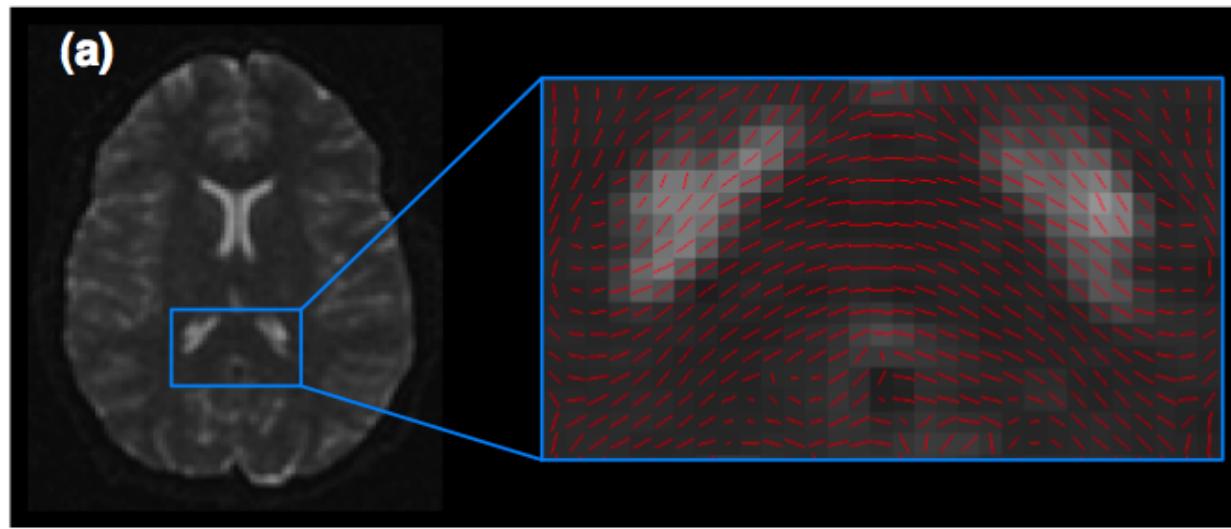
$$D_1 = \lambda_{11} \mathbf{m}_1 \mathbf{m}_1^T + \lambda_{21} (\mathbf{p} \mathbf{p}^T + \mathbf{q} \mathbf{q}^T)$$

eigenvectors:  $\mathbf{m}, \mathbf{p}, \mathbf{q}$

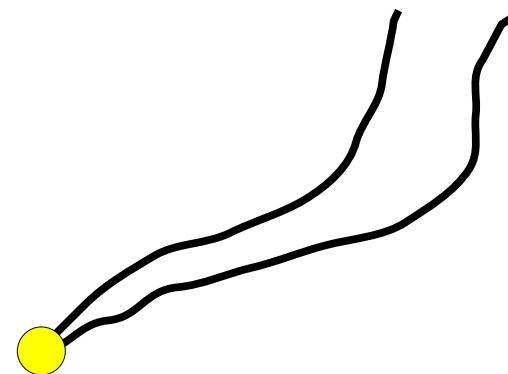
# method: estimating the model

*IPMI* 2009  
*MICCAI* 2009

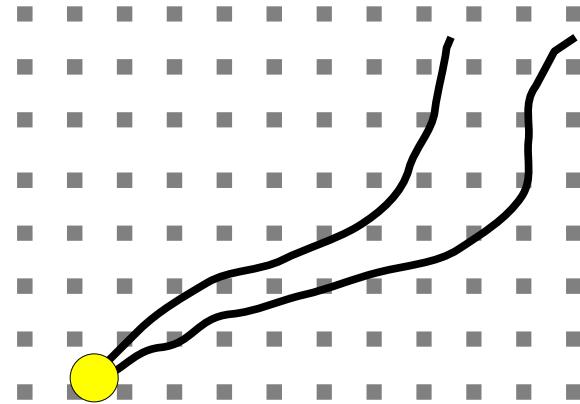
# independent estimation



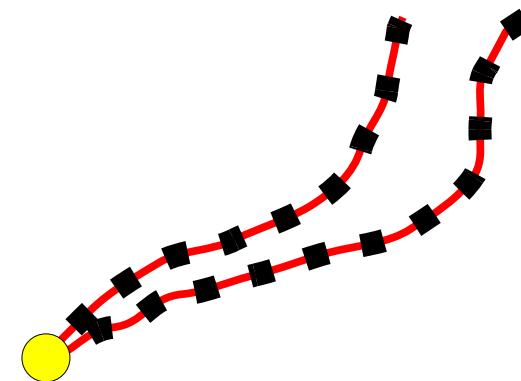
# the system: a fiber



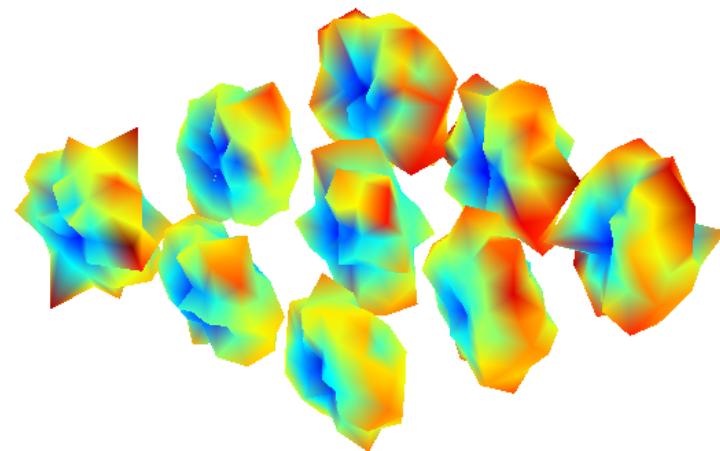
**independent  
process**



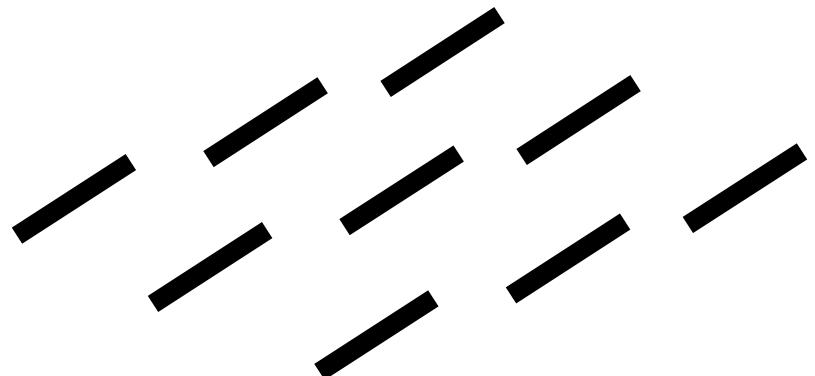
**causal  
process**



# model-based filtering



scanner  
measurement



underlying  
model

objectives:

- estimate model from measurements
- suppress noise

# notation

$\boldsymbol{x}_t$  state of system at time  $t$   
state = “model  
parameters”

$\boldsymbol{y}_t$  what you see at time  $t$   
observation,  
measurement

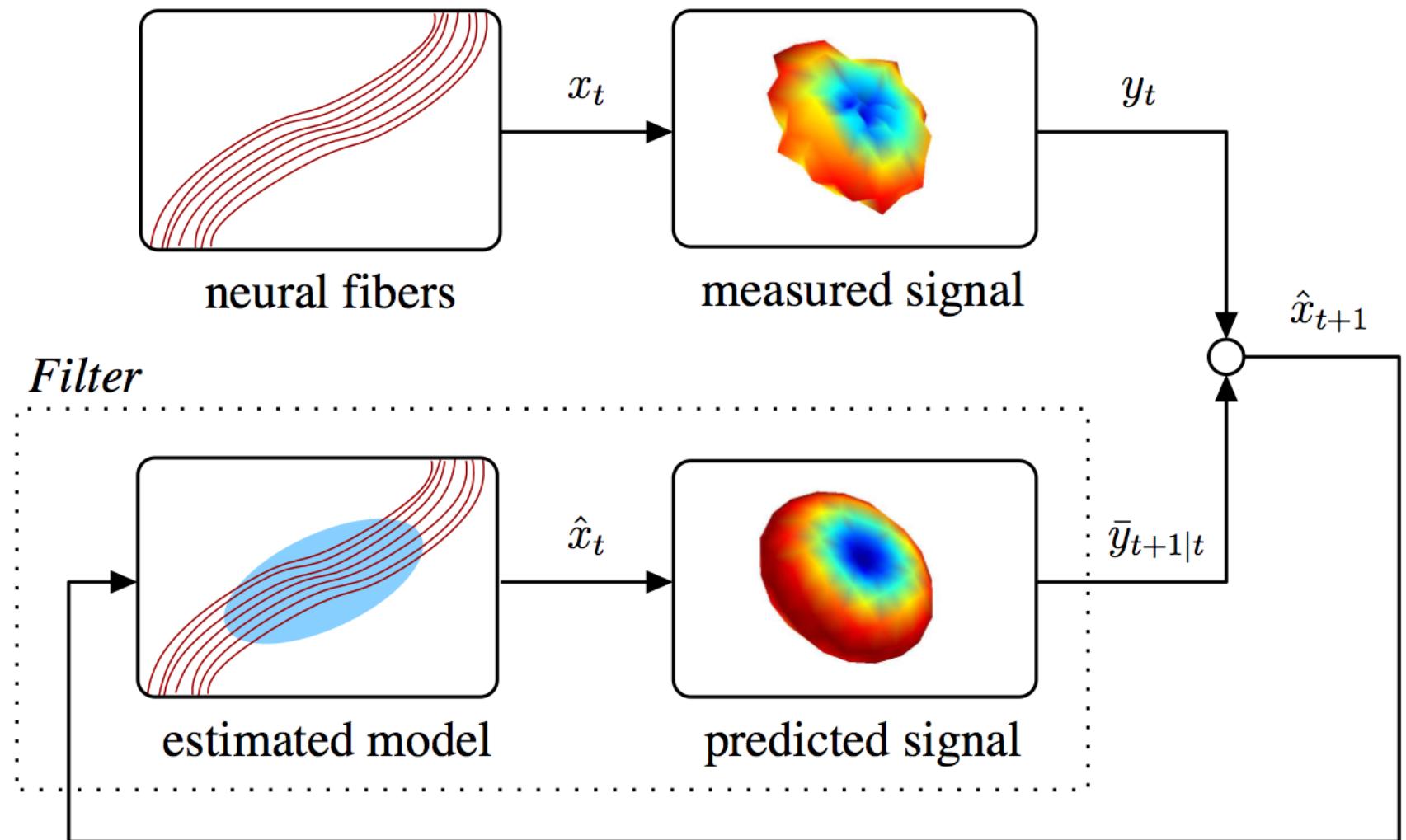
update:       $\boldsymbol{x}_{t+1} = F \boldsymbol{x}_t$        $\boldsymbol{x}_{t+1} = f(\boldsymbol{x}_t)$

observation:     $\boldsymbol{y}_t = G \boldsymbol{x}_t$        $\boldsymbol{y}_t = g(\boldsymbol{x}_t)$

linear

nonlinear

# Kalman filtering



predict ... measure ... reconcile ... repeat ...

$$\begin{aligned} \boldsymbol{x} &= [\boldsymbol{m}_1 \lambda_{11} \lambda_{12} \boldsymbol{m}_2 \lambda_{21} \lambda_{22}]^T \in R^{10} \\ y &\in R^m \text{ signal} \quad \begin{matrix} 10 \text{ dimensional} \\ \text{state} \end{matrix} \end{aligned}$$

$$\boldsymbol{x} = [\boldsymbol{m}_1 \lambda_{11} \lambda_{12} \boldsymbol{m}_2 \lambda_{21} \lambda_{22}]^T \in R^{10}$$

10 dimensional  
state

$$y \in R^m \text{ signal}$$

$$\boldsymbol{x}_{t+1} = f(\boldsymbol{x}_t) = \boldsymbol{x}_t$$

small steps  
slowly varying  
state

$$y_t = g(\boldsymbol{x}_t) = S(\boldsymbol{u})$$

$$\boldsymbol{x} = [\boldsymbol{m}_1 \lambda_{11} \lambda_{12} \boldsymbol{m}_2 \lambda_{21} \lambda_{22}]^T \in R^{10}$$

$$y \in R^m \text{ signal}$$

10 dimensional  
state

$$\boldsymbol{x}_{t+1} = f(\boldsymbol{x}_t) = \boldsymbol{x}_t$$

small steps  
slowly varying  
state

$$y_t = g(\boldsymbol{x}_t) = S(\boldsymbol{u})$$

$$y(\boldsymbol{u}) = S(\boldsymbol{u}) = 0.5 s_0 e^{-b\boldsymbol{u}^T D_1 \boldsymbol{u}} + 0.5 s_0 e^{-b\boldsymbol{u}^T D_2 \boldsymbol{u}}$$

$$D = \lambda_1 \boldsymbol{m} \boldsymbol{m}^T + \lambda_2 (\boldsymbol{p} \boldsymbol{p}^T + \boldsymbol{q} \boldsymbol{q}^T)$$

# signal reconstruction is nonlinear

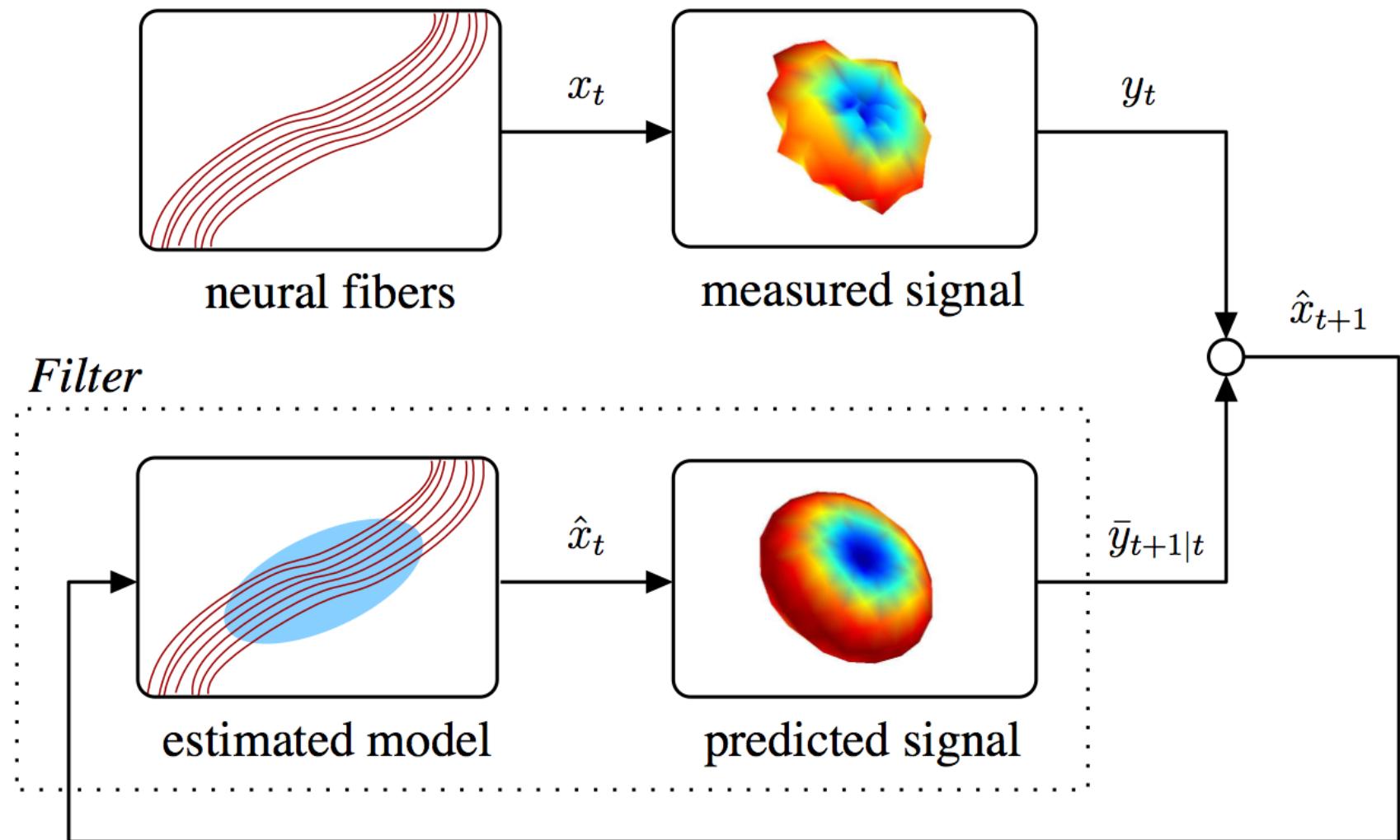
## independent optimization

- least squares  
*linearization*
- gradient descent  
*local minima*
- Levenberg-Marquardt  
*local minima*

## causal estimation

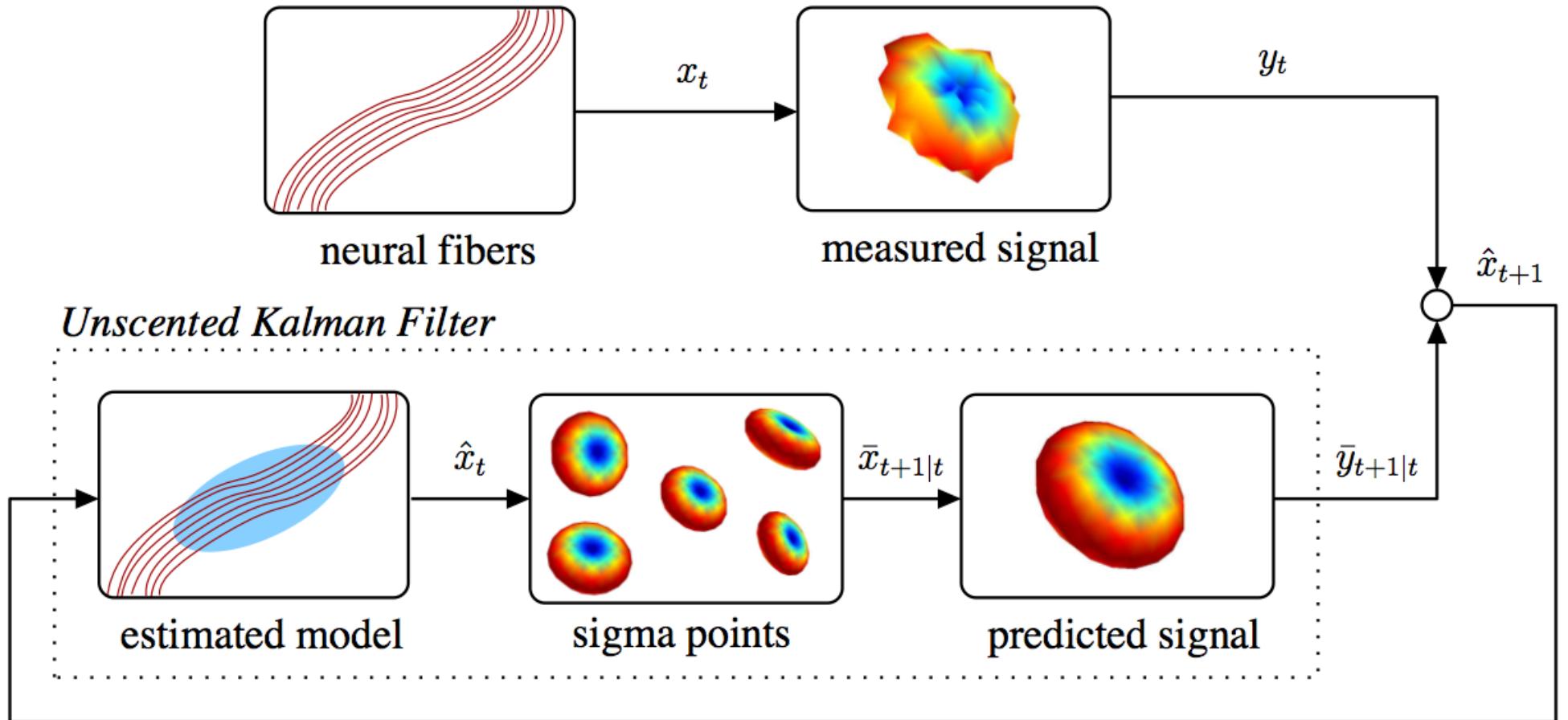
- extended Kalman filter  
mean + covariance  
*linearization*
- particle filter  
non-parametric  
*sampling*
- unscented Kalman filter  
mean + covariance  
no linearization  
limited sampling

# linear Kalman filter



predict ... measure ... reconcile ... repeat ...

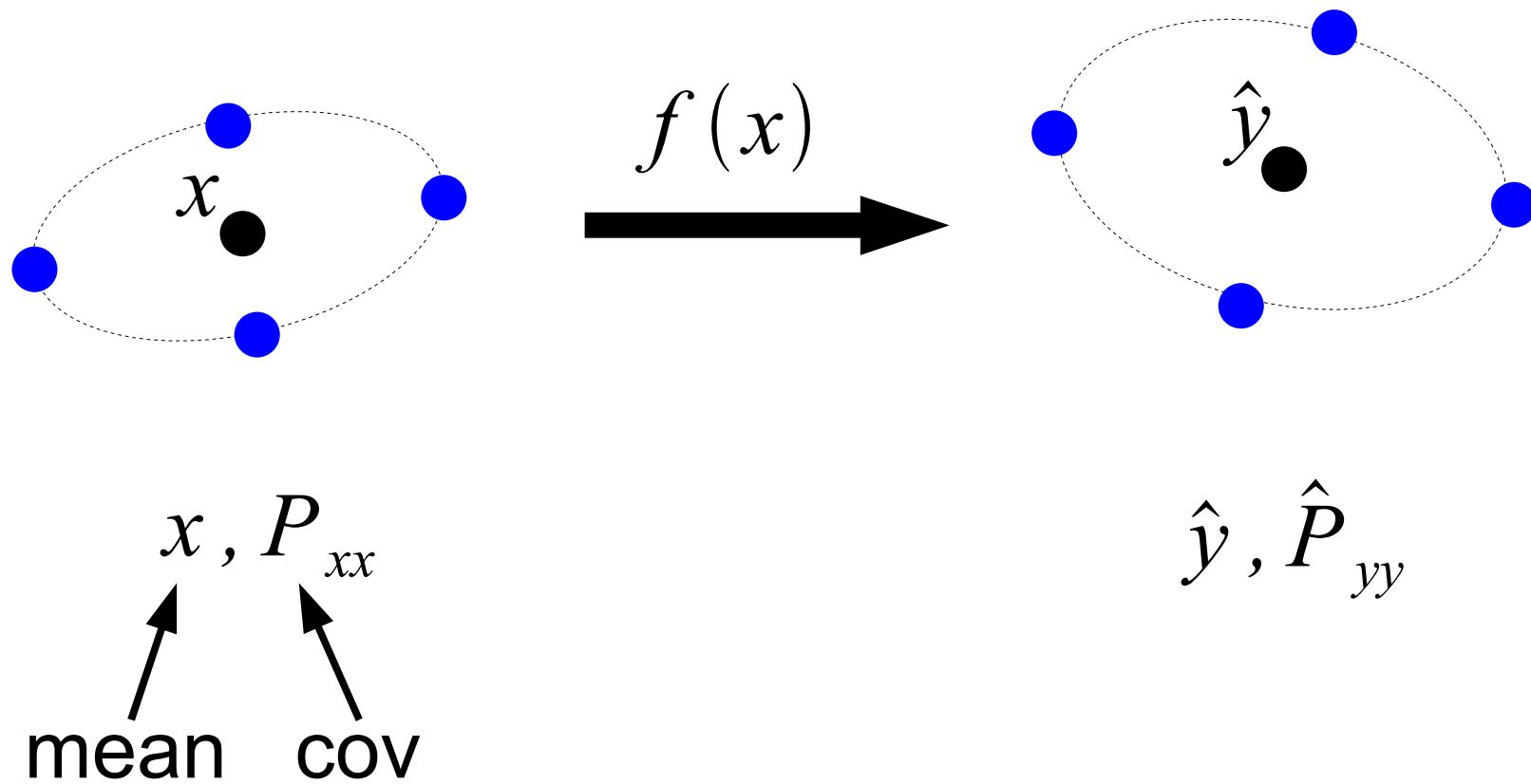
# unscented Kalman filter



same update equations  
modified prediction step

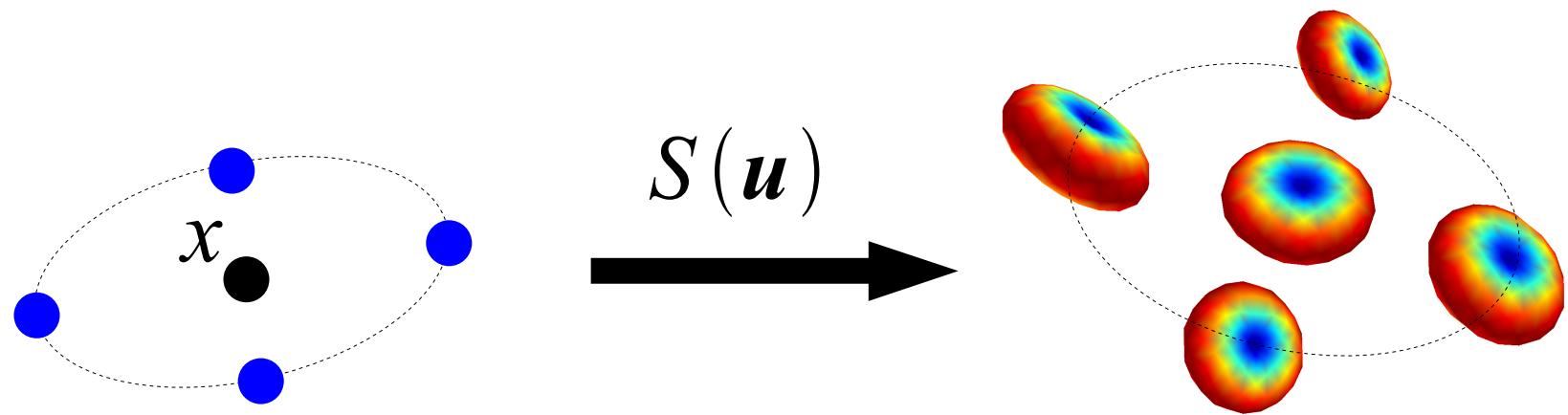
# unscented transform

approximate the statistics...not the function



# unscented transform

for signal reconstruction...

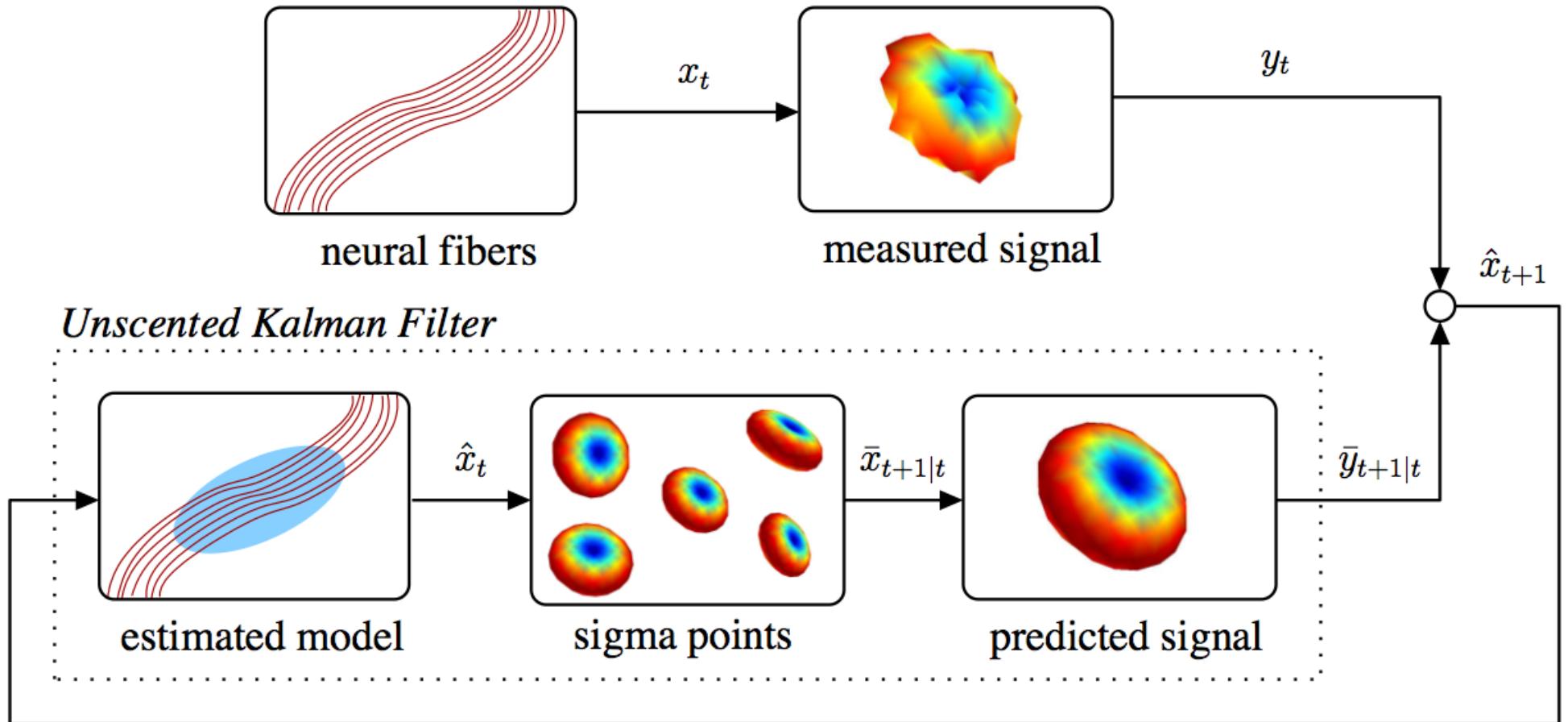


$$x, P_{xx}$$

$$\hat{y}, \hat{P}_{yy}$$

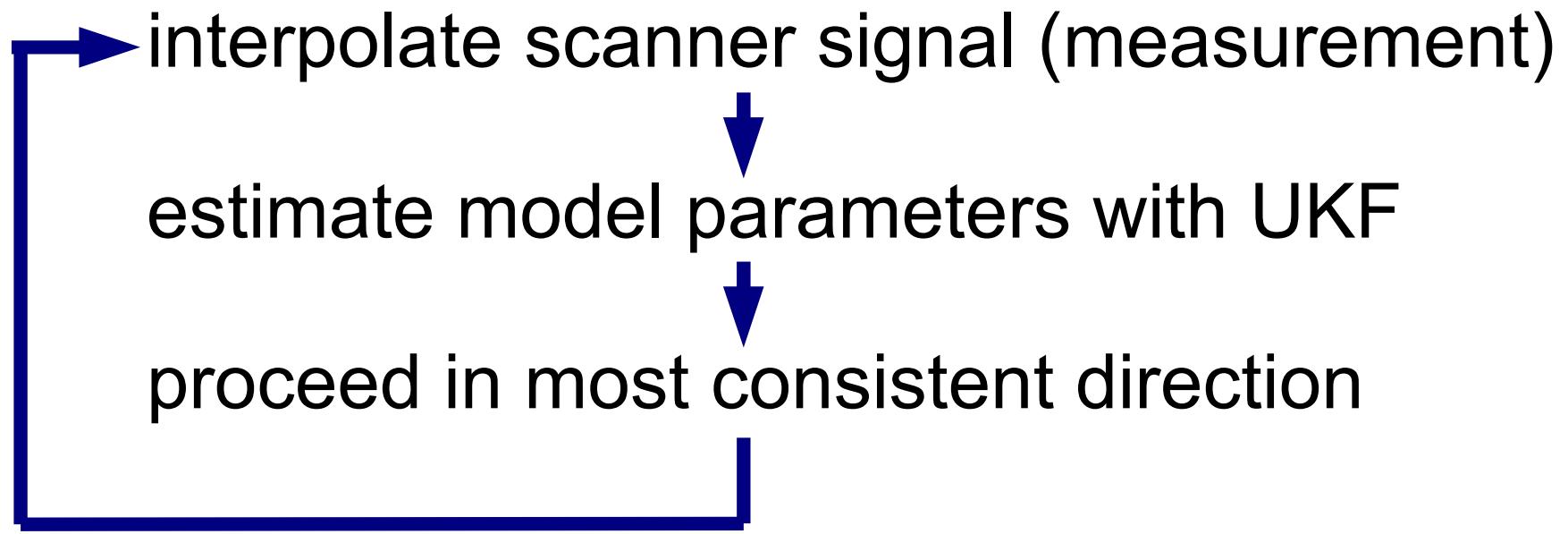
$$x = [\mathbf{m}_1 \lambda_{11} \lambda_{12} \mathbf{m}_2 \lambda_{21} \lambda_{22}]^T$$

# unscented Kalman filter



predict ... measure ... reconcile ... repeat ...

# algorithm



terminate:  $FA < 0.15$

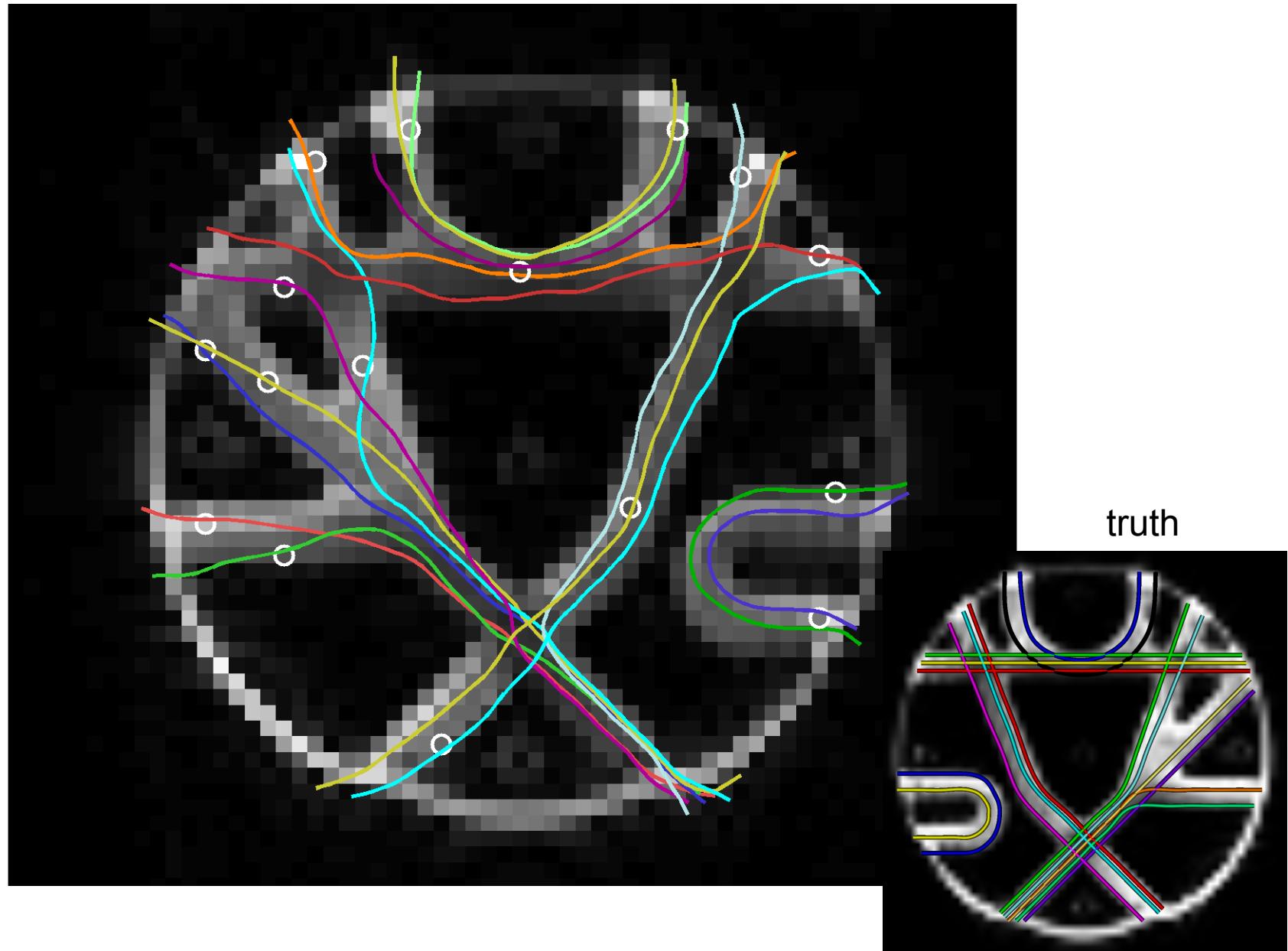
# the phantom

- 1)Seed throughout the mask (“full brain”)
- 2)Select fibers passing through seed points
- 3)Manually select representative fiber

b=1500, 3mm

# the phantom

3mm  
 $b=1500$



# conclusion

inherent coherence along the fiber

we should exploit it in the estimation

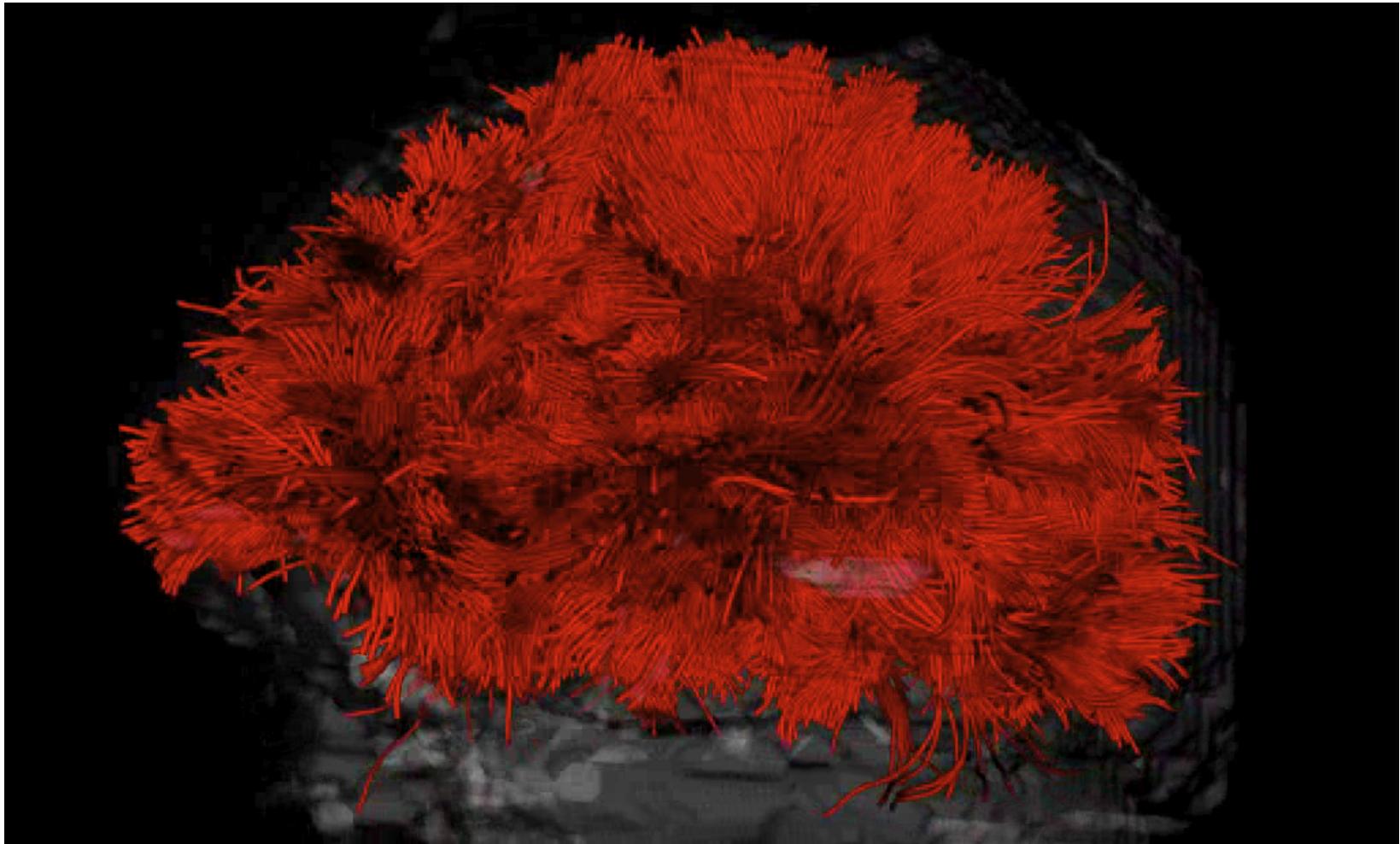
# Connectivity Studies

- Discrete paths
  - Pros: fast, tract-based studies
  - Cons: easily go off-track
- Probabilistic connectivity
  - Pros: handle uncertainty
  - Cons: leaking, difficult to interpret
- Filtered tractography
  - Accurate local estimates (mean, cov)
  - Probabilistic tractography

# Local vs. Global

- Local methods easy go off track
- Global methods often over-regularize path
- Anatomic priors
- Hybrid
  - local: signal-model
  - global: path
- Filtered tractography
  - Replace local streamline in sampling
  - Covariance uncertainty indicates failure

end



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